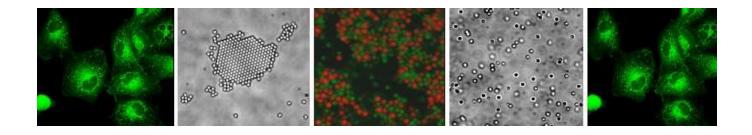
### **Dissecting Cell Rheology and Active Stress Fluctuations**

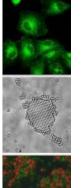


### John C. Crocker

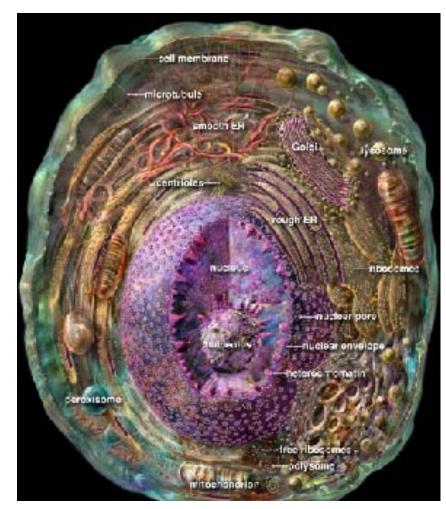
Chemical and Biomolecular Engineering



Krumhansl Symposium Bangalore 7 FEB 2012



### A cartoon cell

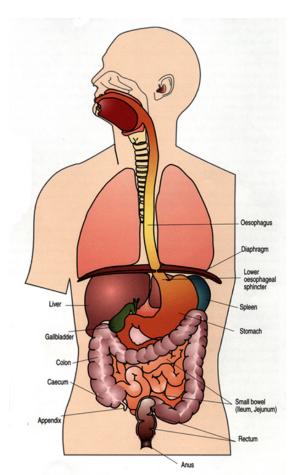


- A passive blob?
- A biochemical factory?
- A complex fluid or simple gel?

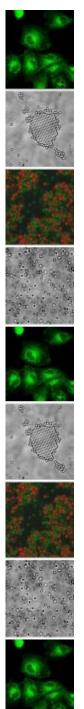
What is 'cell biophysics' good for?





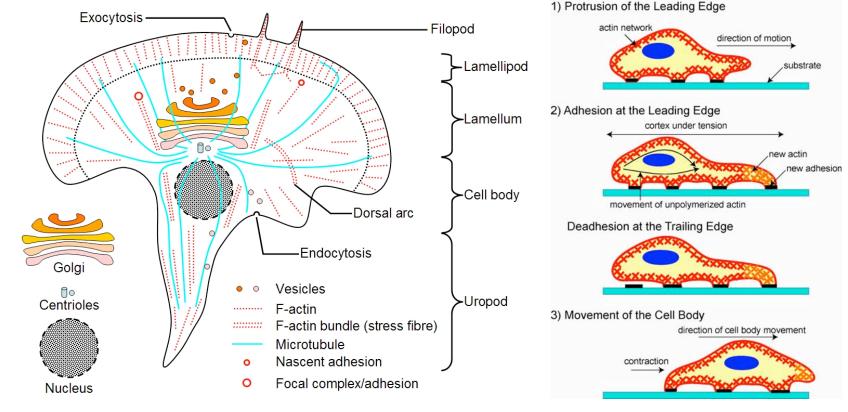


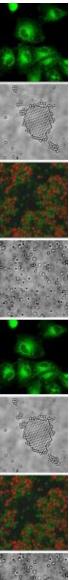
- Skeleton, musculature, brain, omitted
- Both cartoons show biochemical apparatus

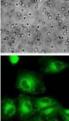


### The Real Cell...

is a complex mechanical system driven by a biochemical metabolism, nanotech parts and ..... soft matter physics.

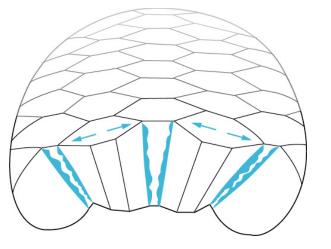


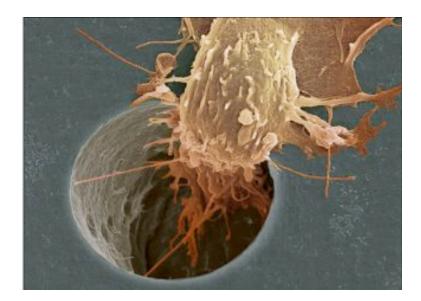






is a versatile, reprogrammable soft *robot*, capable of assembling complex tissues and navigating in 3d by integrating *sensory data* and performing simple computation....



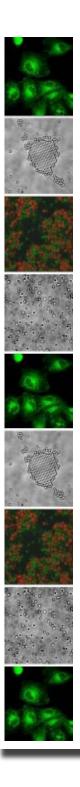


# **Big Picture**

Cells interact with each other and their environment mechanically, sensing hydrodynamic stress, static tension, local stiffness .... by largely unknown means

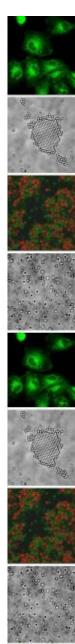
Our failure to understand cell mechanics and mechanosensing impedes progress on major biomedical problems...

Tissue engineering, stem cell therapy, cancer...



### First Step

Understanding how stress propagates within and deforms cells is a *prerequisite* for understanding their bio-mechanics and ultimately their mechano-sensing.

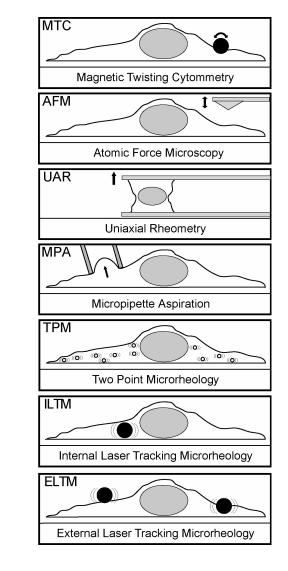




### Plan/Outline

- I. Background
- **II. Different Challenges**
- III. Find a consensus rheology
- IV. Molecular roles in rheology
- V. Active gel behavior

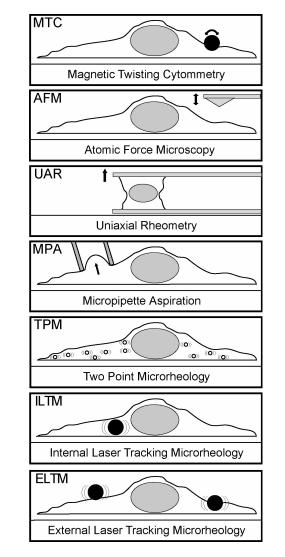
# Cell Rheology Methods



Many methods in use, some for a century (!) Geometries and deformation fields are 'complicated', requiring modeling

Before ~2000: cells are either hard, soft, elastic, viscous, or viscoelastic (!)

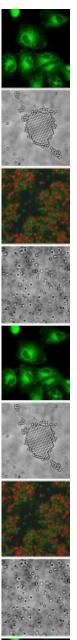




Last decade: 'power-law fluid', very little agreement on stiffness or treatment effects

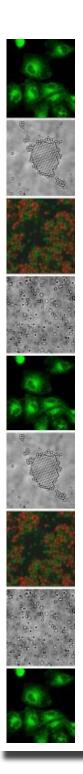
Results do NOT look like simple gels of purified filaments.

No proper physical model(s) (yet)!



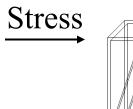
### Toward a consensus

- Hypothesis: A cell contains distinct mechanical structures having different stiffness and rheology, and different methods may probe different structures.
- Approach: Compare multiple methods on a single cell population.



# Rheology (Active Method)

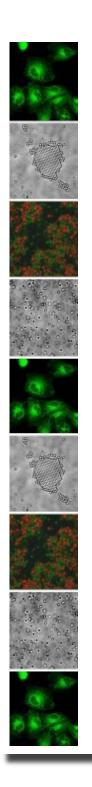
Measure dynamic shear modulus G(ω), a dynamic resistance to deformation



Ι

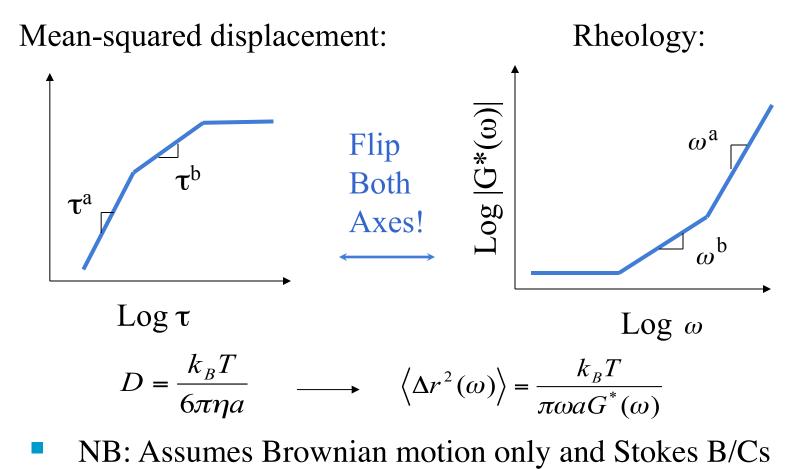
 $\gamma = \frac{1}{L}$   $\sigma e^{i\omega t} = G^*(\omega)\gamma e^{i\omega t}$   $G'(\omega) = \operatorname{Re}(G^*(\omega)) \text{ Elastic Component}$   $G''(\omega) = \operatorname{Im}(G^*(\omega)) \text{ Viscous Component}$ 

Spectroscopic information about microscopic dynamics



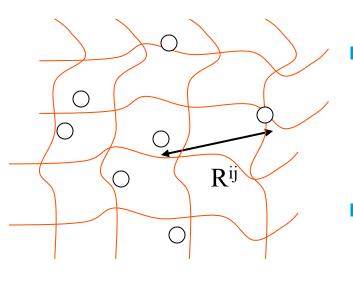
# Rheology (Passive Method)

 Measure the Brownian motion of embedded or attached tracer particles.....



Mason/Weitz, Schmidt/Mackintosh, mid-90s

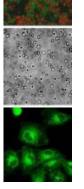
### Two-point microrheology (TPM) Correlate the random motion of two tracers...



Measures the motion of intervening network segment

Insensitive to tracer b/c's!

Two Point Covariance Tensor (has 'Stokeslet' form):  $D_{\alpha\beta}(R,\tau) = \left\langle \Delta r_{\alpha}^{i}(t,\tau) \Delta r_{\beta}^{j}(t,\tau) \delta(R-R^{ij}(t)) \right\rangle_{i \neq j,t}$ 



Corresponding displacement

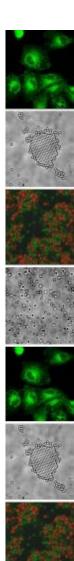
$$\left\langle r^2(\tau) \right\rangle_A = \frac{2R}{a} D_{rr}$$

Levine and Lubensky, PRL 85, 1774 (2000).

Stokes-Einstein Relation

$$D_{rr} = \frac{k_{\scriptscriptstyle B}T}{2\pi\omega RG^*(\omega)}$$

Crocker, et.al., PRL 85, 888 (2000).



### Plan/Outline

### I. Background

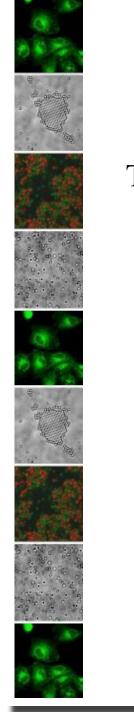
II. Different Challenges

III. Find a consensus rheology

IV. Molecular roles in rheology

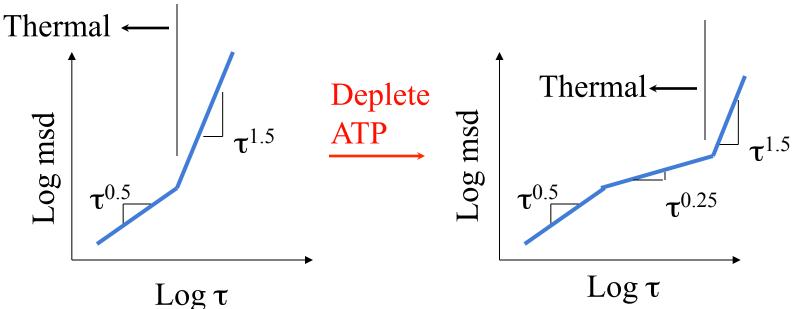
V. Active gel behavior





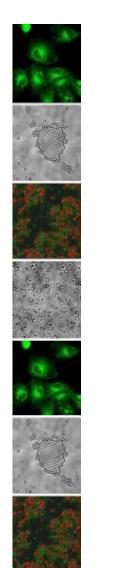
### Challenge 1: Cells are alive

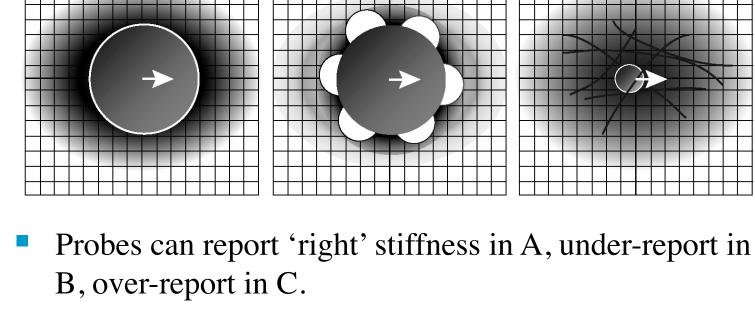
Molecular motors drive 'super-diffusive' motion



Resolution:

- Deplete ATP using azide and deoxyglucose
- 'Super-diffusion' disappears or moves to much longer lag times.
- Use 'thermal' part to compute rheology, do controls.

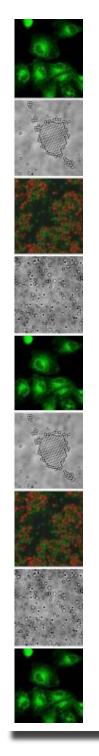


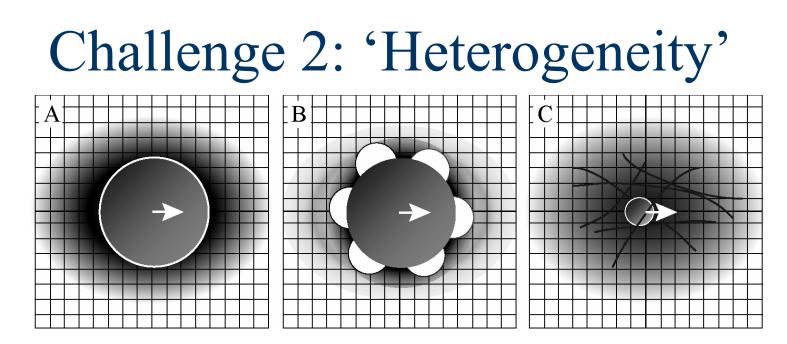


All three cases can have identical frequency dependence

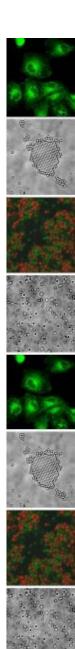
Challenge 2: 'Heterogeneity'







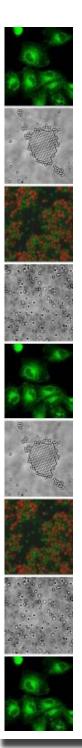
- Probes can report 'right' stiffness in A, under-report in B, over-report in C.
- All three cases can have identical frequency dependence
   Resolution:
- Rely on frequency dependence, discount stiffness.
- Use deformation mapping or 'two-point' microrheology



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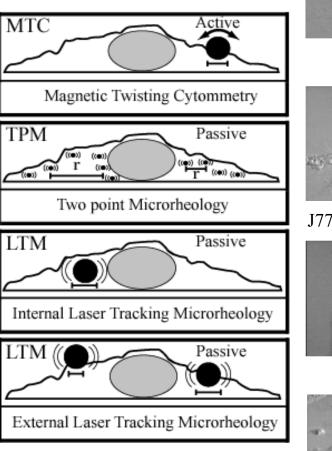
### **Experimental Approach**

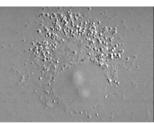
#### Use multiple methods:

- Internal/External
- Active/Passive
- Wide frequency range

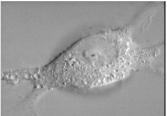


- Image particle tracking
- Laser deflection tracking
- Applied magnetic field

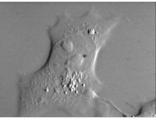




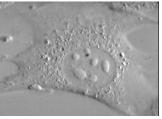
#### TC7 Epithelial



J774A.1 'Macrophage'

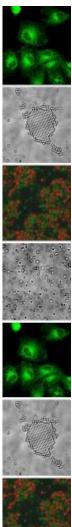


F9 Carcinoma



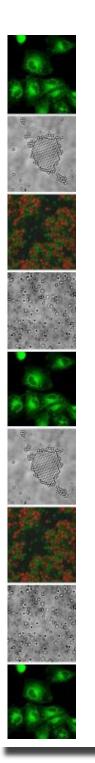
NIH 3T3 Fibroblast

### Questions

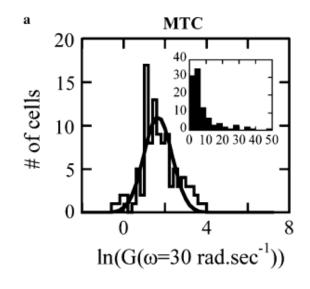


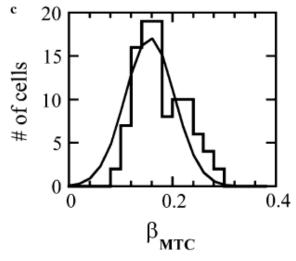
- Does a given method give reproducible results?
- Do different methods agree?
- Compare to literature?





### Magnetic Twisting Cytometry



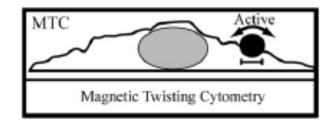


Rocking amplitudes are log-normal distribution amplitudes vary by > decade

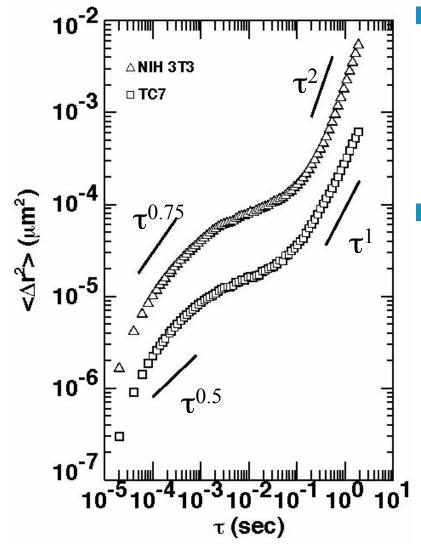
Power-law fluid:

 $G(\omega) \sim \omega^{\beta}$ 

Frequency dependence
 IS consistent from tracer
 to tracer and over time

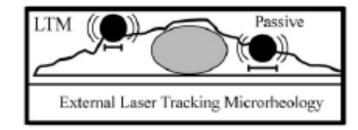


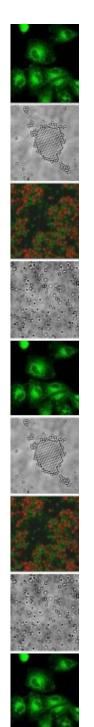
### External LTM (passive motion)



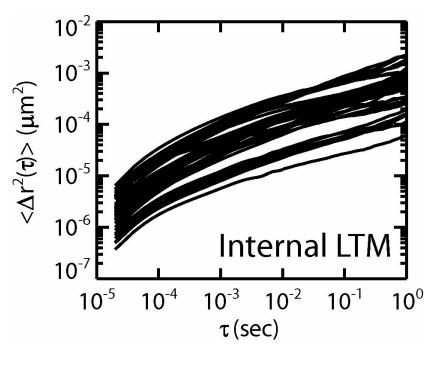
 Long time superdiffusion: random crawling or drift (need to deplete ATP)
 Frequency dependence NOT consistent from tracer to tracer

amplitudes vary by > decade





### Internal LTM (passive motion)



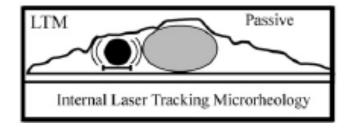
ATP depleted

Intermediate times consistent with powerlaw fluid:

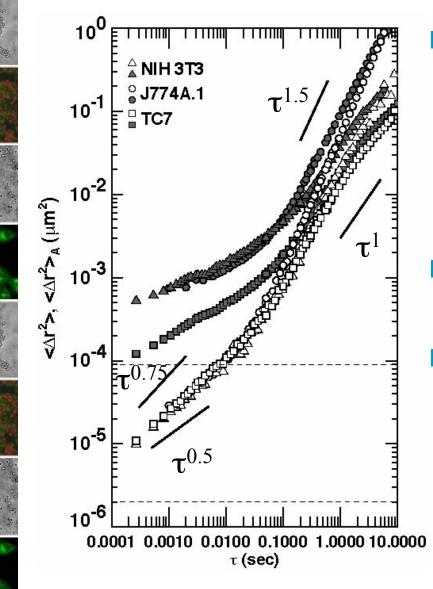
 $msd \sim t^{\beta}$ 

Frequency dependence IS consistent from tracer to tracer

amplitudes vary by > decade



### **Two-Point Microrheology**

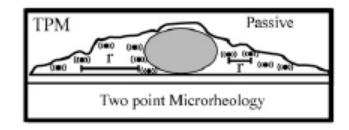


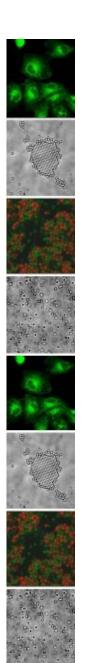
Large 1-point/ 2-point difference.....

heterogeneity: either spatial or of B/Cs

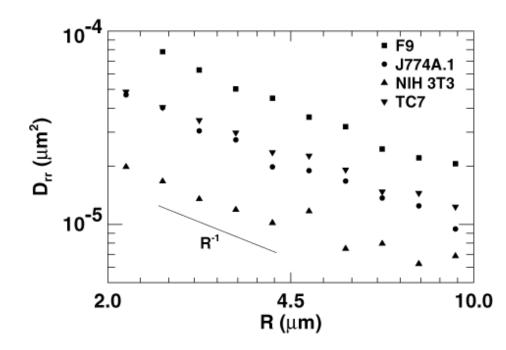
Amplitude similar b/w cells and cell types!

Super-diffusive at long times: ATP depletion

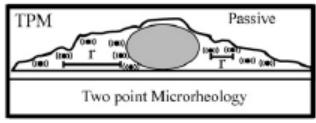




### TPM Continuum check

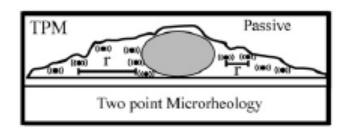


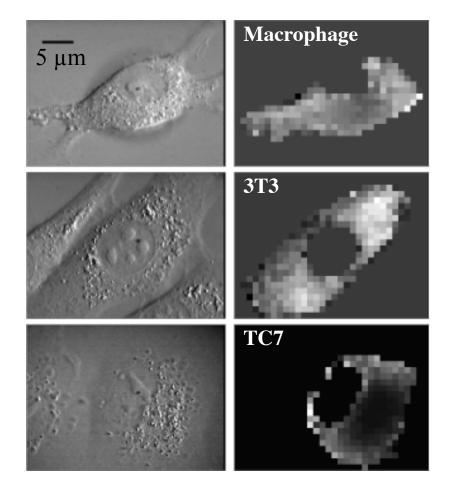
- 1/R decay in D<sub>rr</sub> indicates 3D continuum
- Not sensitive to micron scale heterogeneity or weak spatial gradients

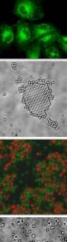


# Two-point mapping

- Strain maps differ among cell types
- Contrast between interior and edge factor of 2x or so
- Dark region is rough endoplasmic reticulum (RER)











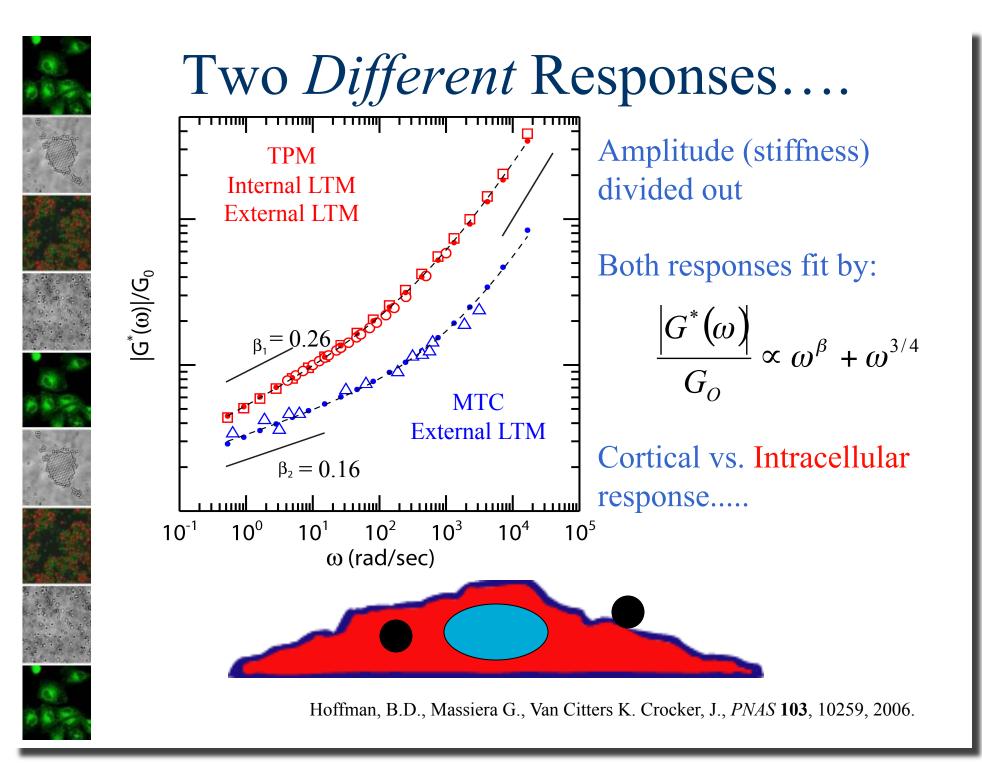




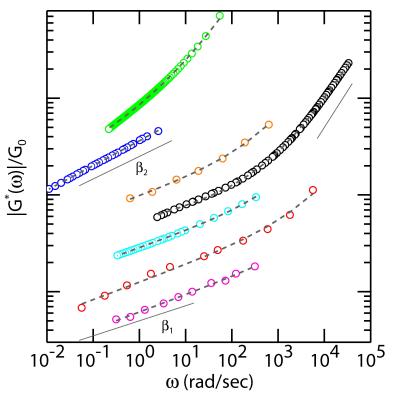




### Do the four techniques agree?



### Comparison to Literature



• All fit by:  $|G^*(\omega)| \propto \omega^{\beta} + \omega^{3/4}$ 

All active experiments:

- External Bead Pulling Feneberg, et. al BJ, 2004
- Uniaxial Rheometer Desprat, et. al., BJ, 2005

• AFM

Alcaraz, et. al., BJ, 2003

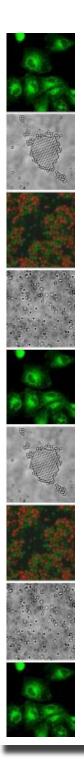
• 'Lamella' LTM Yamada, et. al., BJ, 2000

• External Bead Twisting Creep Lenormand, et. al., J. R. Soc. Lond. Interface

• MTC Fabry, et. al., PRL, 2001

- External Bead Laser Trapping Balland, et. al., European BJ, 2005
- Also fit into two groups of exponent values, cortical/ deep interior
- Caveat: Grouping may be spurious: two different structures may have similar rheology.

Hoffman, B.D., Massiera G., Van Citters K. Crocker, J., PNAS 103, 10259, 2006.

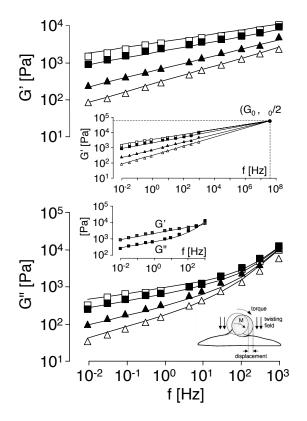


# A Universal description?

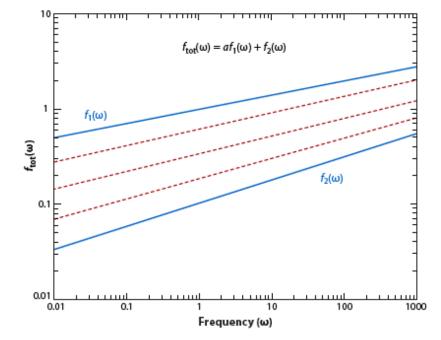
- Cells are "power-law fluids":
  - $G^*(\omega) = G_0 \left(\frac{\omega}{\omega_0}\right)^{\beta}$  + viscosity
- Five decade range
- Exponent is continuously distributed: 0.1<β<0.25</p>

SGR Theory ?!

Fabry et al., Phys. Rev. Lett. 87, 148102 (2001).

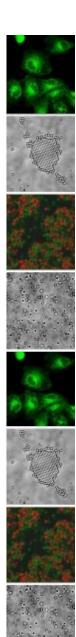


# Challenge 3: Power-law math



Linear superposition of two weak power-laws creates 'intermediate power-law exponents'!

- Family of cross-over curves extrapolate to a point
- May be unreliable to use exponents as 'fingerprints' for identifying mechanical structures.
- Might see a composite result -> need to 'dissect'.

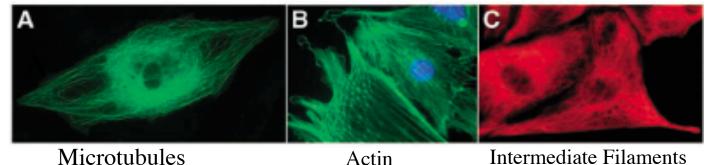


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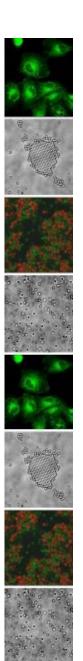


Ingber, JCS, 2003



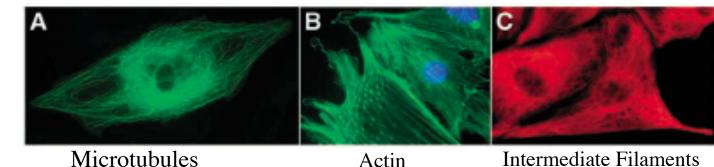
- Actin Network
- Microtubules
- Intermediate filaments (keratin, vimentin, etc)
- Stress fiber network (actin-myosin)
- Smooth ER (bicontinuous lipid tubule network)
- Rough ER, Golgi (lamellar lipid stacks)

Approach: biochemical perturbation rather than mechanical 'dissection'



### The Choices....

Ingber, JCS, 2003



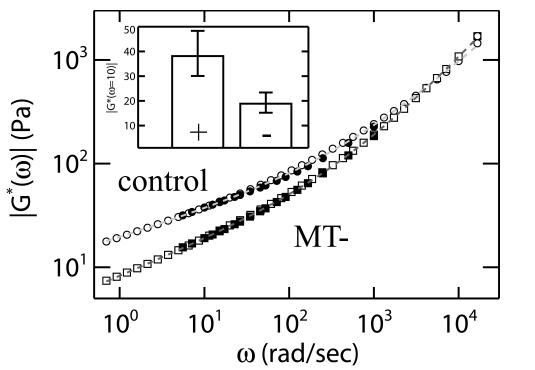
- Actin Network
- Microtubules
- Intermediate filaments
- Stress fiber network
- Smooth ER
- Rough ER, Golgi

Latrunculin A Colchicine

- Gene knockout?
- Blebbistatin
- M $\beta$ CD ?
- Brefeldin A?

Challenges: 2+ separate structures/compartments, networks are interconnected, cells can 'adapt'..... Do 4 measurements per treatment and a lot of controls/interpretation.

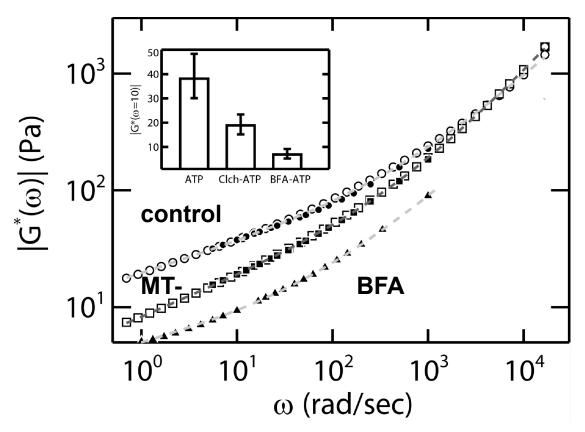
# MT disruption (interior)



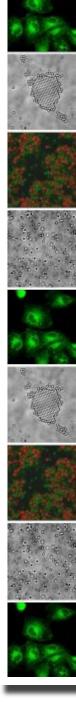
TPM + LTM (int)

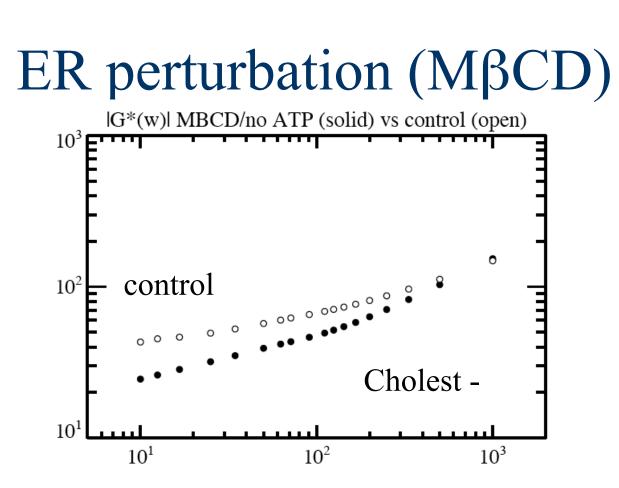
- Colchicine 10 µM, ATP depleted. (Staining not shown)
- Roughly a 2X softening at 10 rad/sec, (p<0.01).</p>
- Different exponents in fit, 0.26->0.33.
- Suggests a mechanical role for MTs, but not only MT.
- No cortical effect (not shown)

## ER perturbation (BFA)

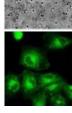


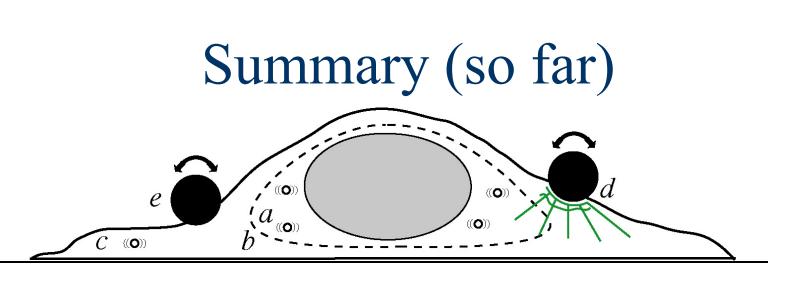
- ER perturbation with BFA leads to 3X softening (interior).
- Softening appears frequency independent.
- NB: dense membrane systems have power-law rheology.





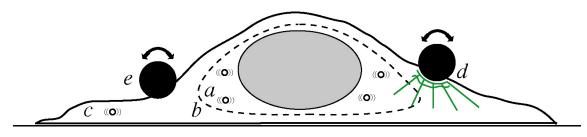
- Cellular cholesterol depleted by methyl-β-cyclodextrin (MβCD)
- Roughly a 2X softening (p<0.05).</p>
- Rheology exponent increases, similar to MT disruption.
- Suggests endomembrane (EndoM) role in stiffness

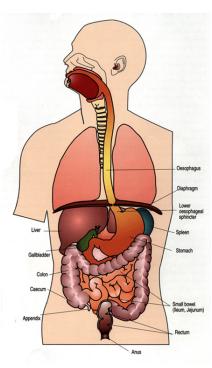


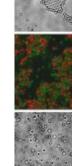


- Three structures: cortex/lamellipodium (b,c), interior (a), and stress fiber network (d).
- Cortex is actin; stress fibers are actin/myosin
- Interior is a complex composite of microtubules and lipid-based structures.
  - Other studies.....
- Little/no IF role in linear rheology
- Nuclear envelope is stiff and has power-law rheology Hoffman BD, Crocker JC, Ann Rev of Biomed Eng, 11, 259-288, 2009.

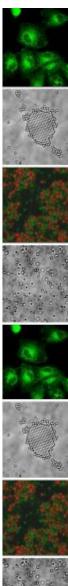
## Summary (so far)





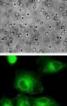


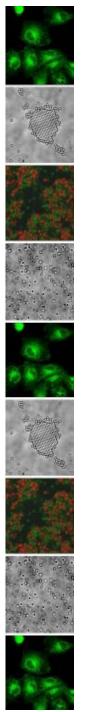
- The functional biomechanical organization of cells resembles that of metazoans:
- Delicate control/shell: brain/skull : nucleus/envelope
- Passive biochemical apparatus: thorax : perinucleus
- Dedicated motility apparatus: musculature : cortex Hoffman BD, Crocker JC, Ann Rev of Biomed Eng, 11, 259-288, 2009.



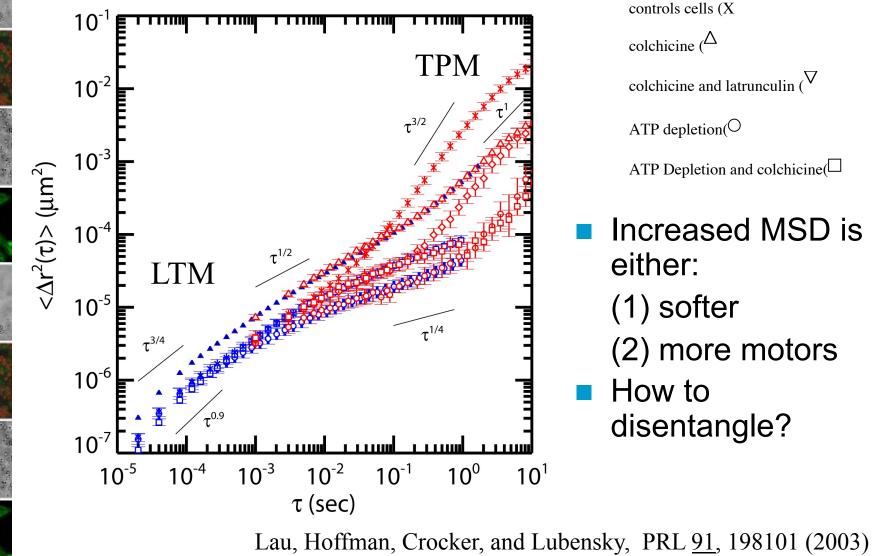
## Plan/Outline

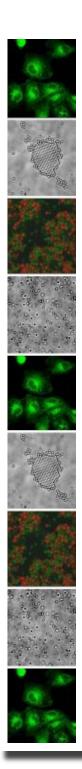
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IV. Molecular roles in rheology
V. Active gel behavior





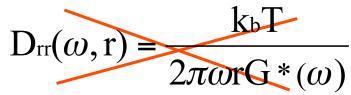
### Active gel behavior of cells





#### Quantifying active fluctuations...

GSER no longer valid in a non-thermal regime

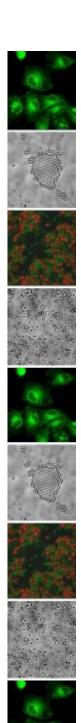


- Two point correlation still valid in an active, driven medium
- Brownian driving replaced by  $\Delta(\omega)$ , Fourier power spectrum of the fluctuating stresses (assume stresslet force dipoles)

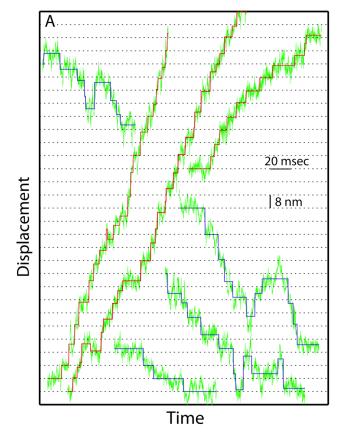
Linear  
Response 
$$strain^2 \propto \frac{stress^2}{|G^*|^2} \longrightarrow D_{rr} = \frac{\Delta(\omega)}{6\pi r |G^*(\omega)|^2}$$

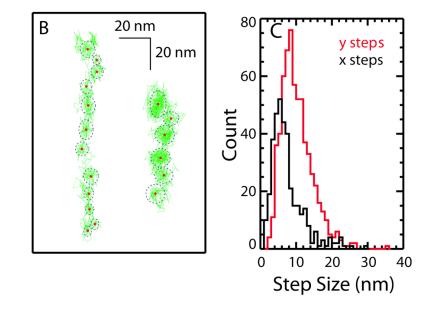
- If we know  $G^*(\omega)$  and  $D_{rr}$  then can compute  $\Delta(\omega)$  ....
- Use ATP depleted cells to get rheology, as before.

Lau, Hoffman, Crocker, and Lubensky, PRL 91, 198101 (2003)

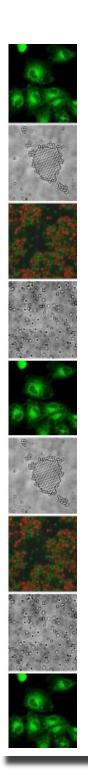


### Contribution #1 Molecular Motors





- Step size and rates match expectations for MT motors
- Inbound (dynein) take larger steps than outbound (kinesin)
- Bidirectional motion from multiple motors ?
- 'Jiggling' between steps is >> tracking error

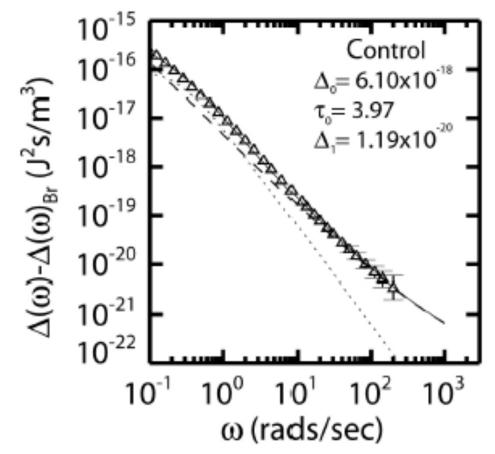


#### Contribution #1 Molecular Motors

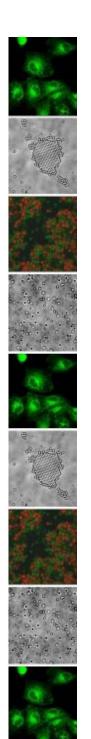
Molecular motor stress steps have ~  $\omega^{-2}$  spectrum, stress kicks have ~  $\omega^{0}$  spectrum. Pulses, mean length  $\tau_{m}$ : Lorentzian w/ corner freq  $1/\tau_{m}$  $\Delta_{m}(\omega) \sim 1/(1 + (\omega \tau_{m})^{2})$ stress  $\int d_{m}(\omega) = 1/(1 + (\omega \tau_{m})^{2})$ 

Contains information about motor timescales...

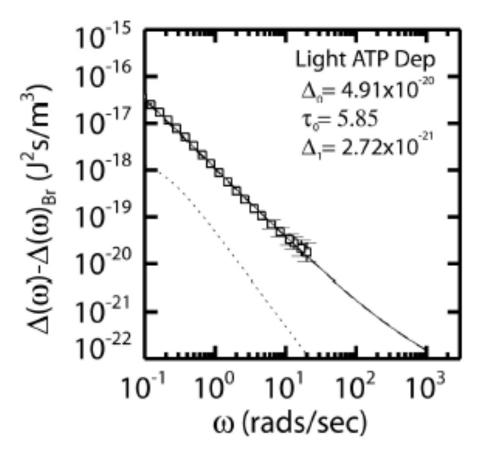
# Stress spectra (normal cells)



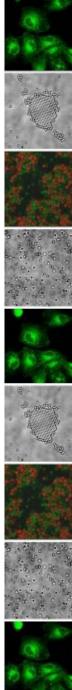
Normal cells require a superposition of Lorentzian and a power law ~ \omega^{-3/2} — two sources? (Brownian subtracted)
 Motor timescale is ~ 4 sec, about right for MT motors such as kinesin



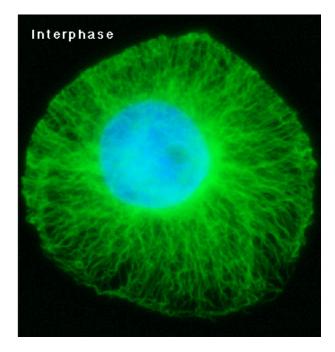
## Stress spectra (slight ATP-)

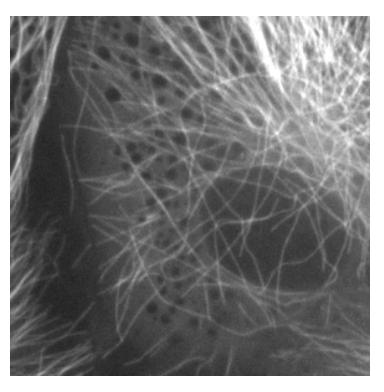


- Partial ATP depletion confirms two distinct sources
- Kinesin processivity is very sensitive to [ATP]
- $\sim \omega^{-3/2}$  fluctuations remain, dominate the spectrum.



#### Contribution #2 MT remodeling

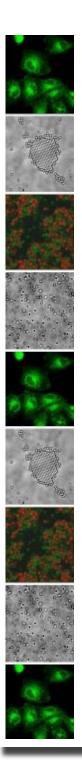




P Wadsworth, UMass



- Bending indicates MT are in stressed configurations
- Stress is applied (released) when MT (de)polymerize



### Contribution #2 MT remodeling

Andy WC Lau, Florida Atlantic University

Assume an active polar gel, having a spatio-temporally varying mean polarization field, obeying the PDE:

$$\partial_t p_i(\mathbf{x},t) = -\tau_p^{-1} [1 - \xi_p^2 \nabla^2] p_i(\mathbf{x},t) + s_i$$

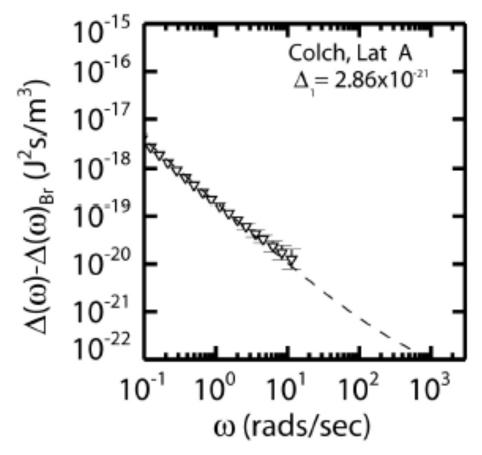
where  $\tau_p$  is a relaxation time due to MT remodeling,  $s_i$ , and  $\xi_p$  is a correlation length due to MT bending.

It can be shown that the TPM stress fluctuations have the form:

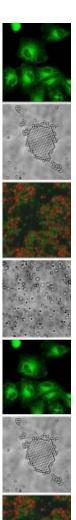
 $\Delta_p(\omega) \sim J(\omega \tau_p / 2)$  where  $J(x) = \frac{\sqrt{1 + \sqrt{1 + x^2}} - \sqrt{2}}{x^2}$ which reduces to  $\Delta_p \sim \omega^{-3/2}$  at high frequencies

Hoffman, Van Citters, Lau, Crocker, submitted

# Stress spectra (MT/actin negative)



- Colchicine and Latrunculin A disrupt MT and actin.
- Weak, ATP dependent residual stress fluctuations....
- Unknown origin, corresponds to simple diffusion in time



# Conclusions

- Animal cells in culture are structured objects, with spatially distinct mechanical subunits seen by different methods.
- Deep interior is a composite of microtubules and lipid structures.
- Stress fluctuations in cells have three distinct sources: MT motors, MT remodeling, and a third unknown source
- Cell subunits all have (different) power-law rheology, suggesting soft glassy dynamics is ubiquitous (but not universal)
- Need new soft matter theories/models.

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Collaborators:

http://crocker.seas.upenn.edu