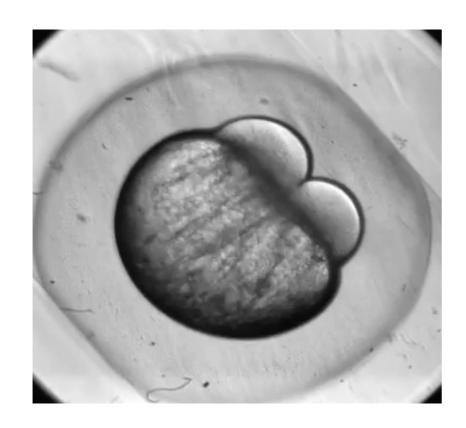
# **Determining Physical Properties of the Cell Cortex**

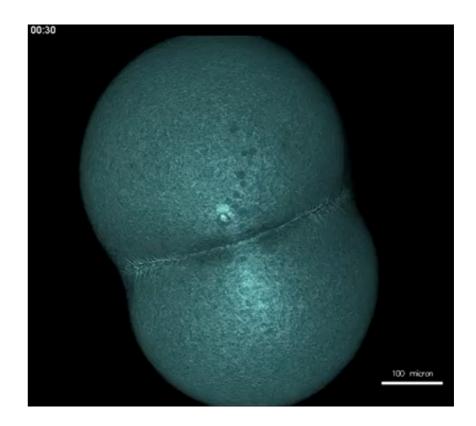
Arnab Saha

Savitribai Phule Pune University (Formerly: University of Pune)

## Zebrafish: Embryonic Development

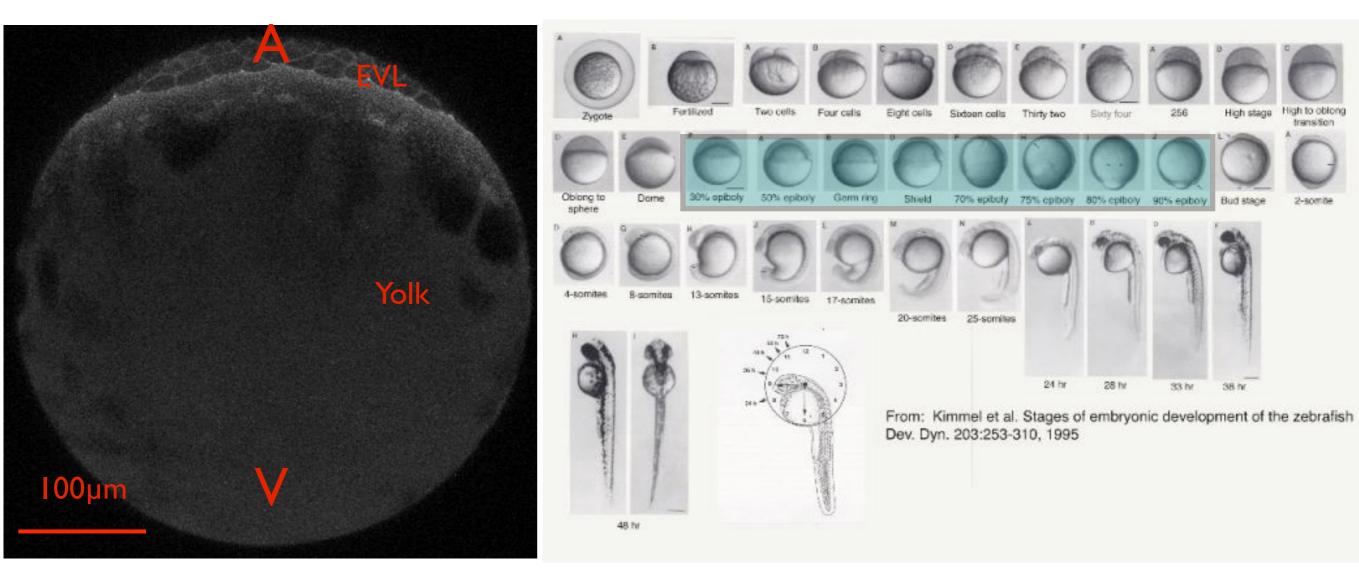






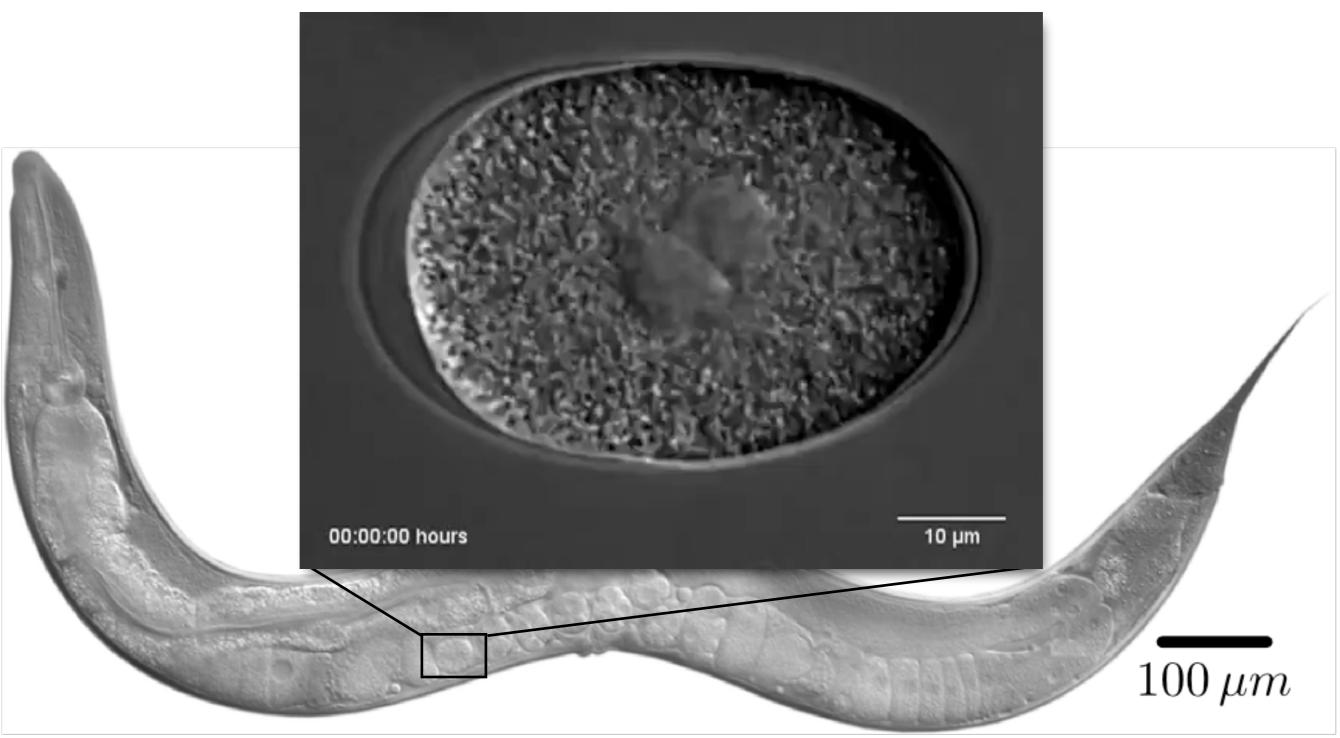
# **Zebrafish Epiboly**





M. Behrndt et. al.Science 338, 257 (2012)

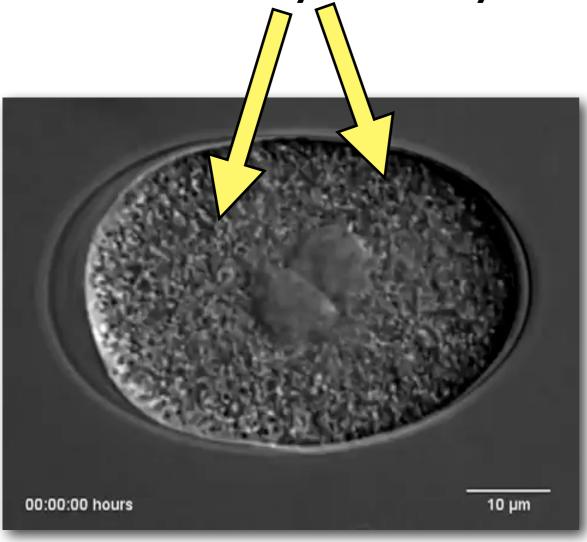
### C. elegans: Embryonic Development



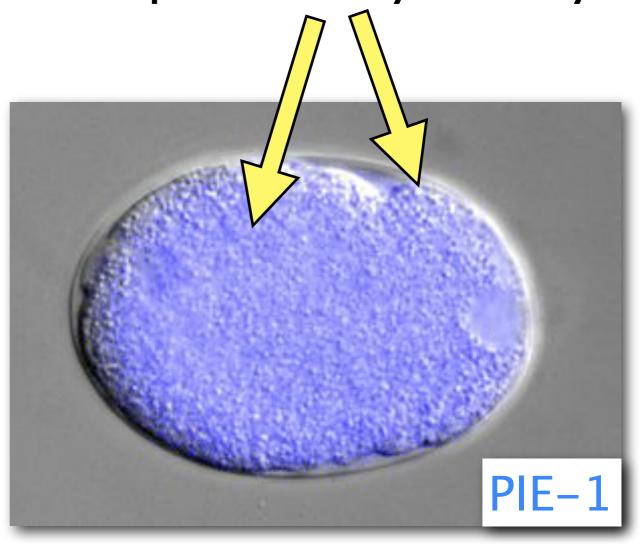
Chin Sang Lab

### C. elegans: Embryonic Development

Size asymmetry

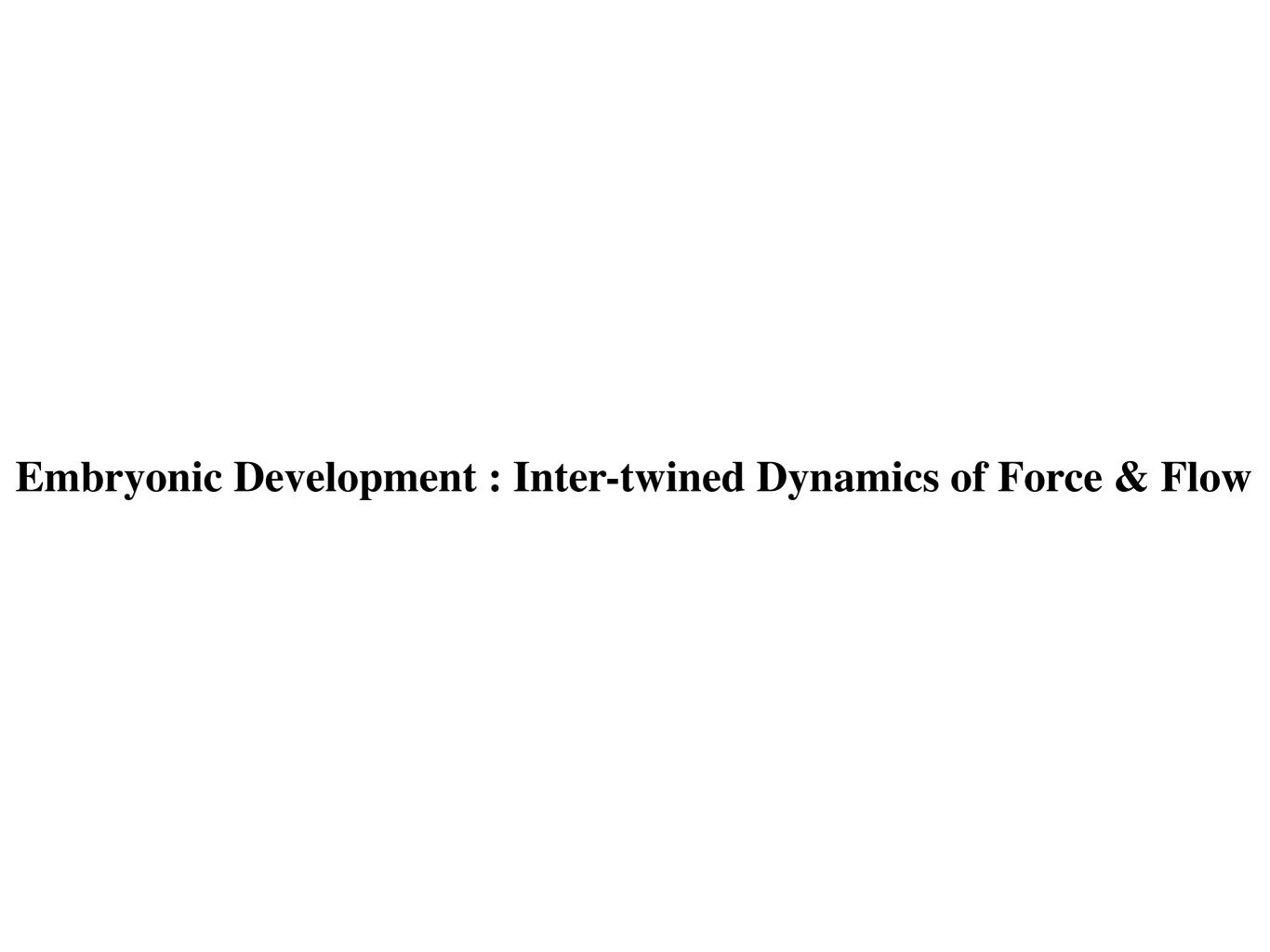


Composition asymmetry

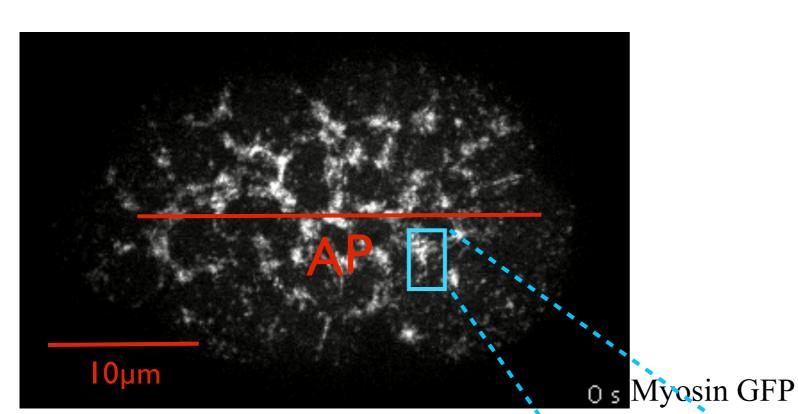


Gönczy and Rose, Wormbook (2005)

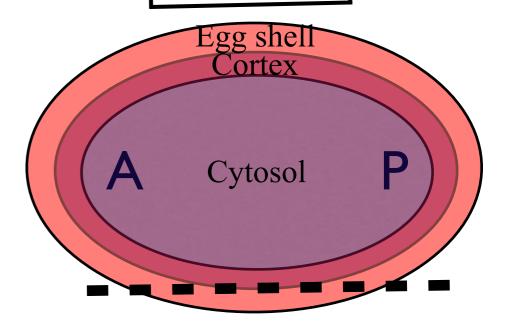
Hyman Lab, MPICBG



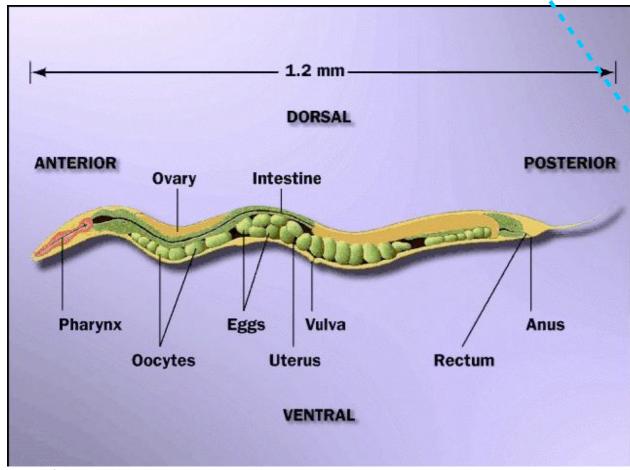
## C. elegans A-P flow



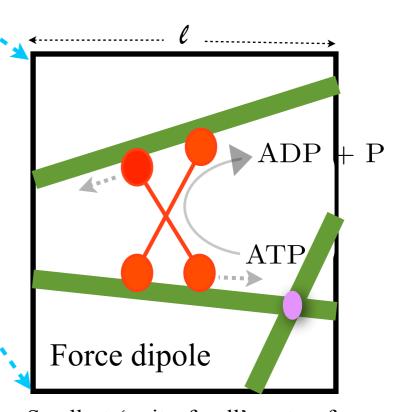
Microscope



Mayer et. al, Nature, 2010.



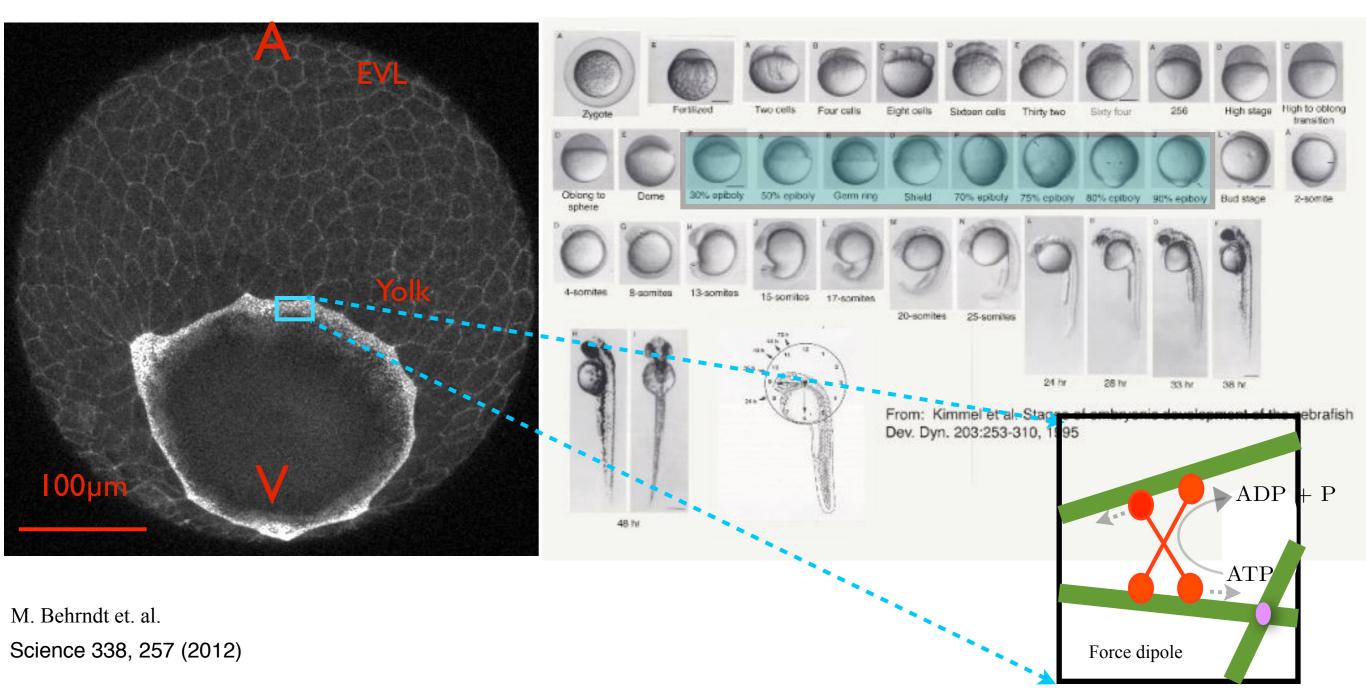
 $\overline{c.elegans} \hspace{0.2cm} \underline{\text{http://www.imsc.res.in/~sitabhra/research/neural/celegans/}}$ 



Smallest 'unit of cell' cortex from molecular scales: Actin, Myosin, Actin Binding Proteins, ATP

# Zebrafish epiboly





# Material Properties of a Fluid Regulate Flow



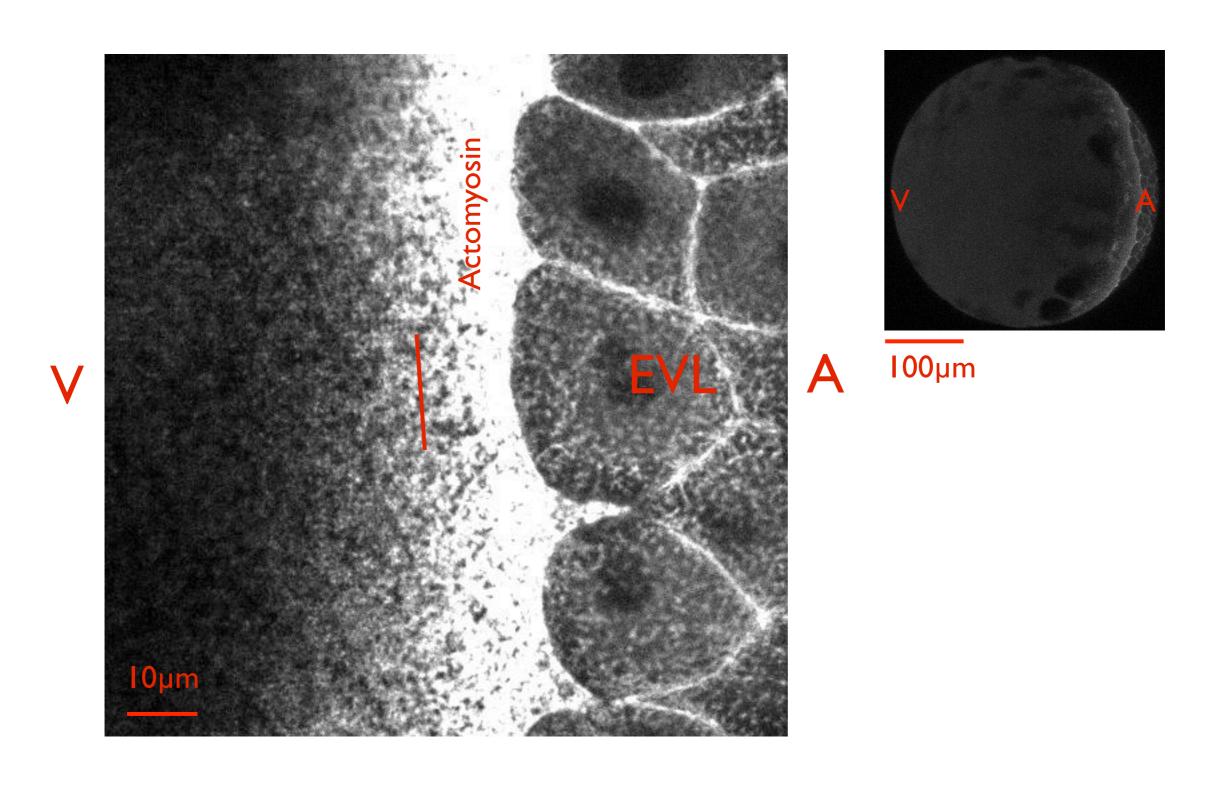
To understand the flow



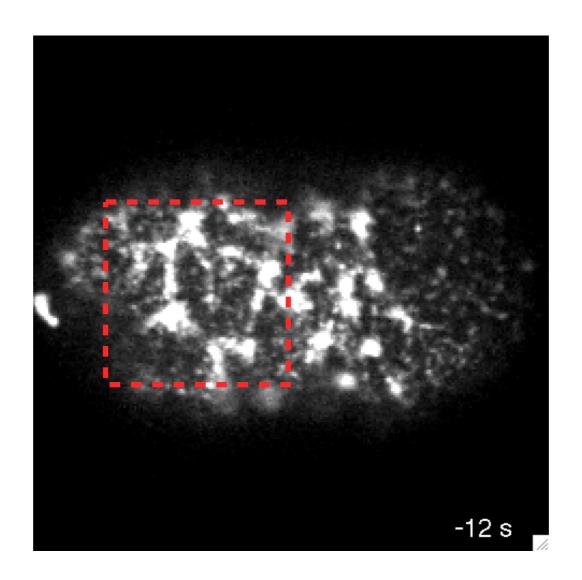
Need to estimate the relevant material properties of the concerned fluid Perturbation to the fluid to estimate the material properties:

Laser ablation

### Laser Ablation: Zebrafish



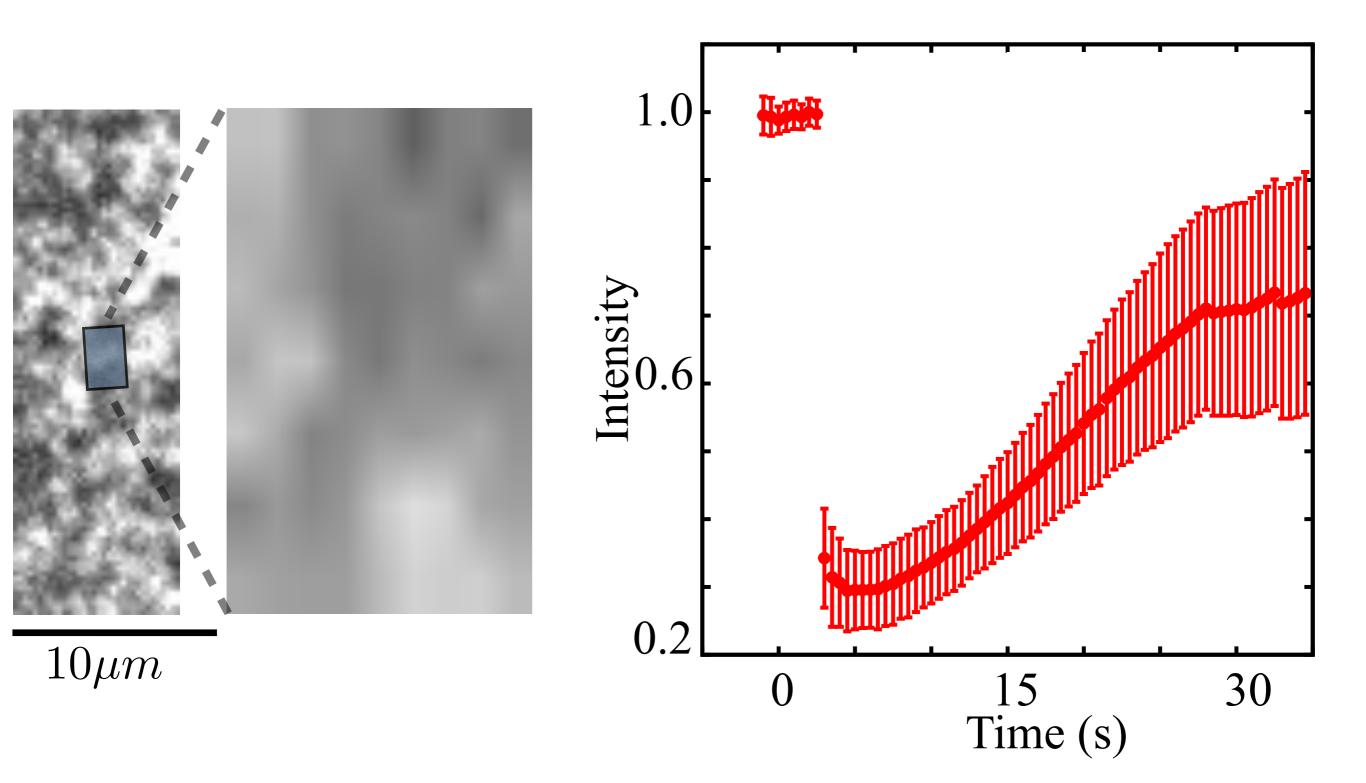
# Laser Ablation: C.elegans



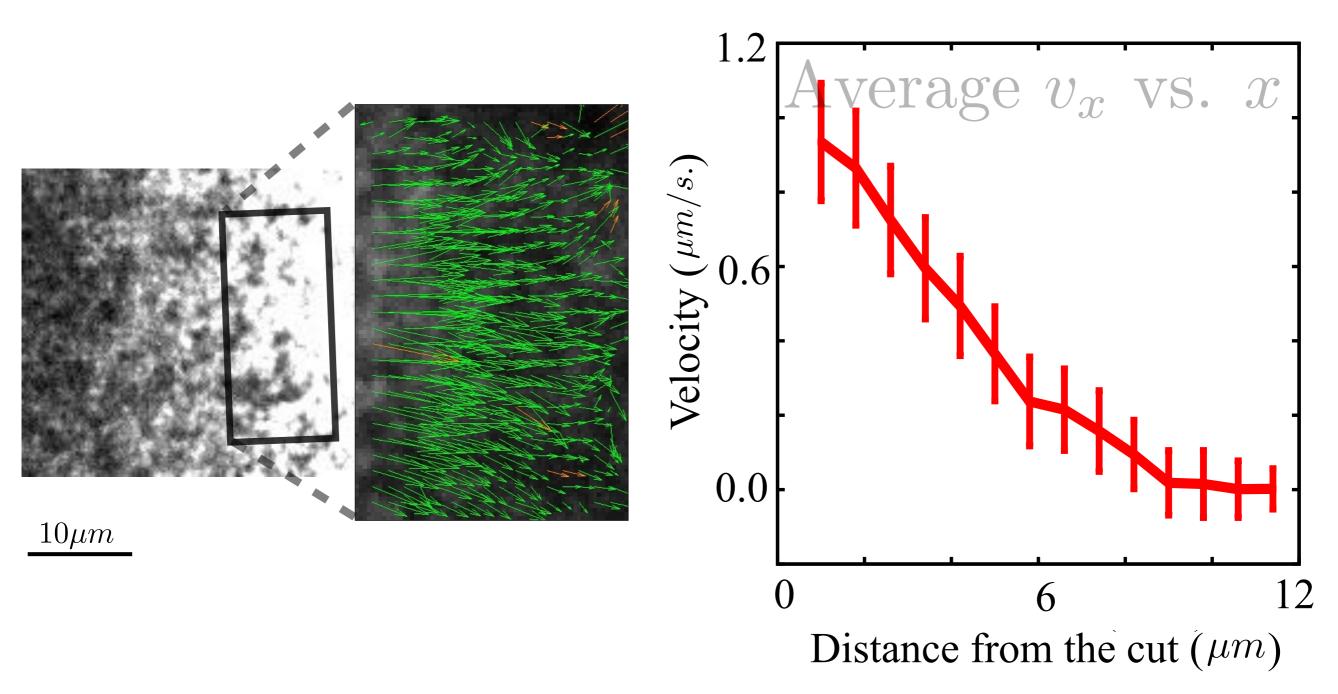
Mayer et. al, Nature, 2010.

Analysis of the	cortical flow	by laser	ablation

Turn-over & on rate

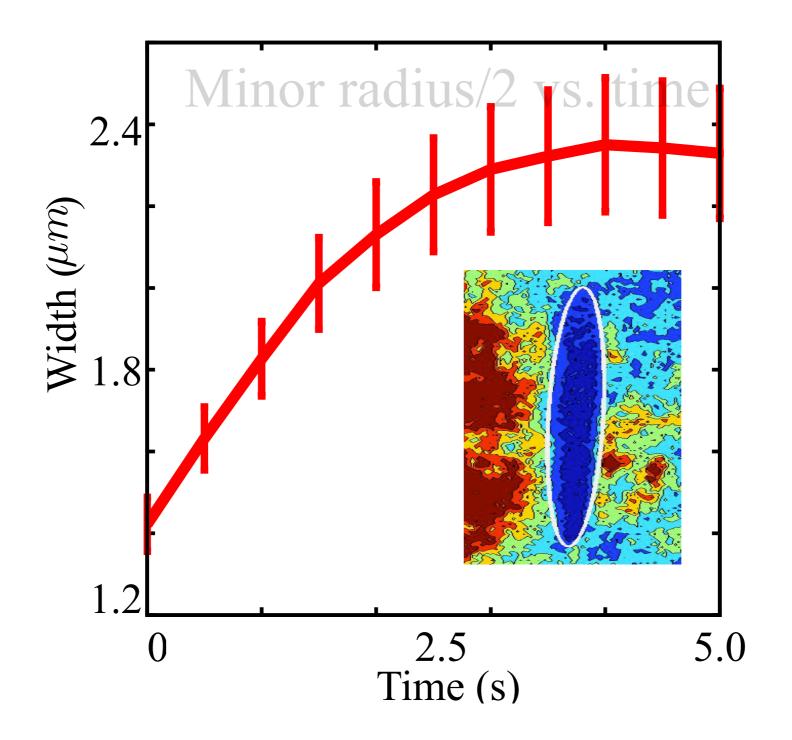


Velocity profile over space

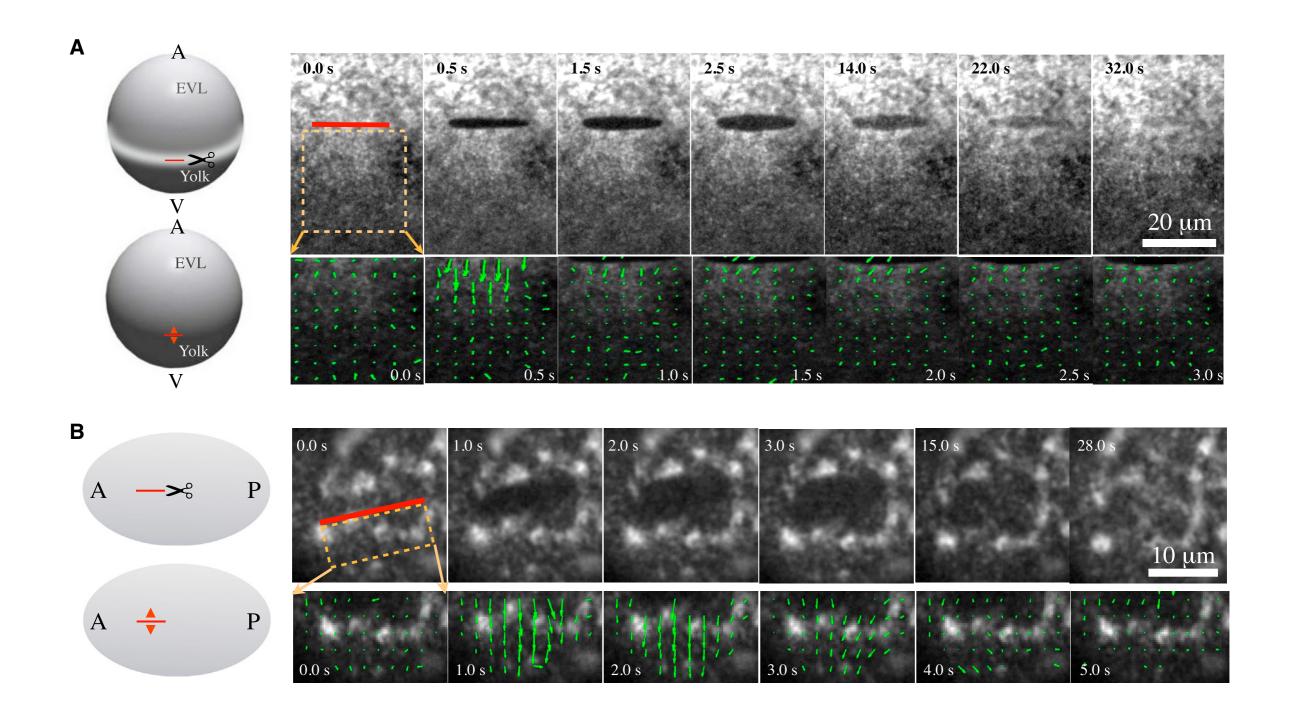


PIV flow field between 1st and 2nd frame (0 to 0.5s)

Width of the hole vs. time

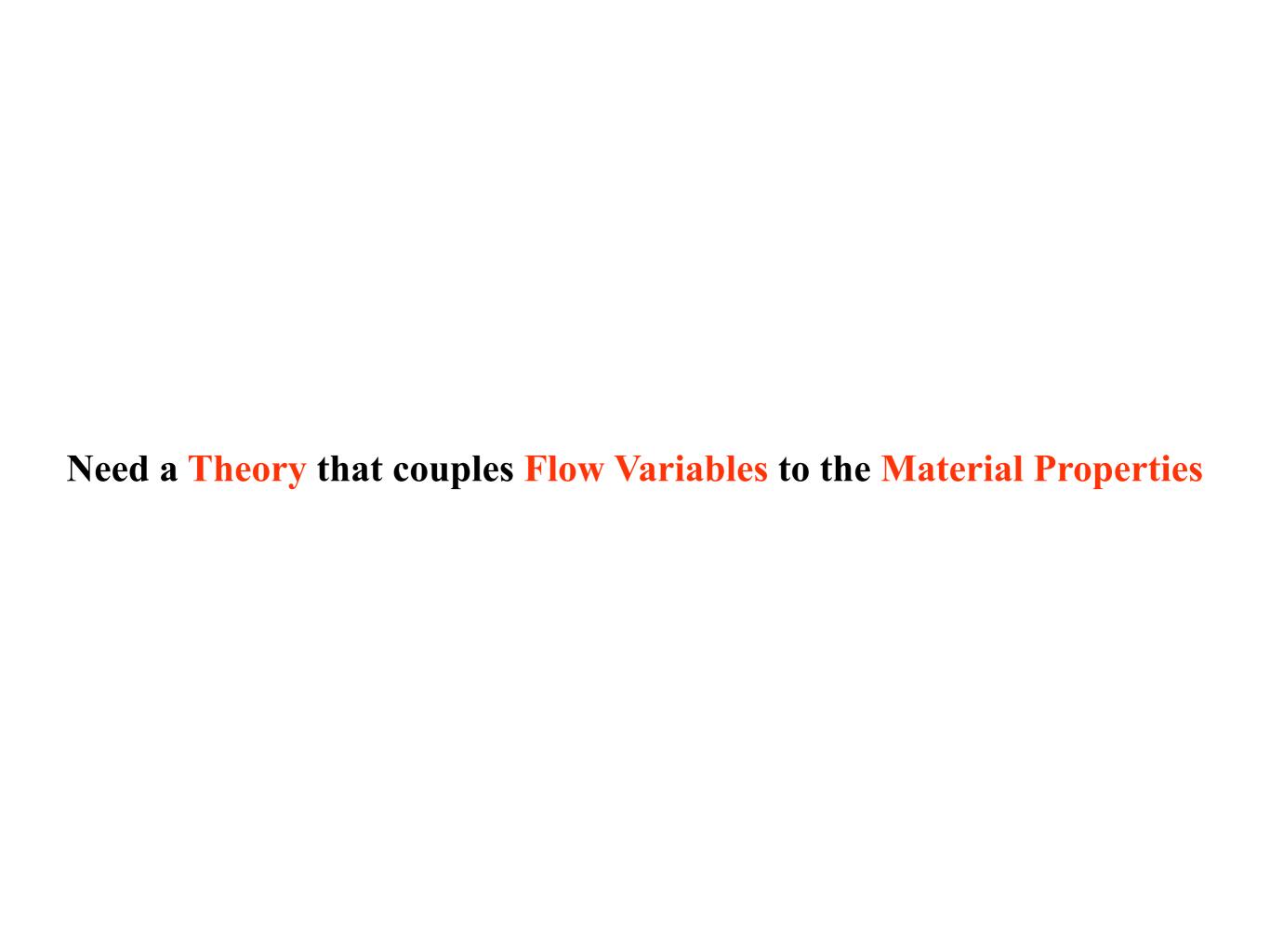


Determine shape of hole as a function of time by thresholding



A. Saha et. al. BJ, 2016

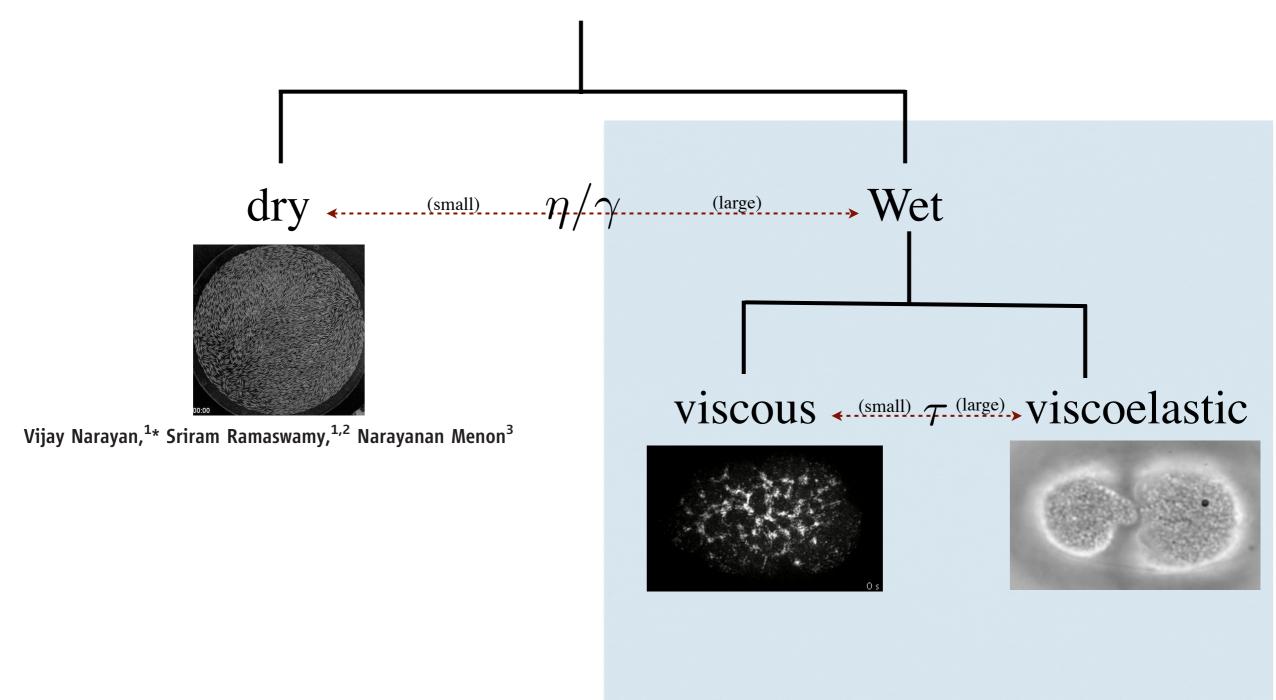
# Analysis of cortical flow Material Properties?



A theoretical description of the general properties of living matter is not currently achievable because of its overall complexity, with the detailed state of a cell determined by a large number of variables.

- Marchetti et. al. RMP (2013)

### 'Active' Matters



### 'Wet' Active Matters or 'Active Gel'

(description of *slightly* active *polar* gel)

$$\frac{\partial g_{\alpha}}{\partial t} + \partial_{\beta} \Pi_{\alpha\beta} = 0,$$

$$\left(\Pi_{\alpha\beta} = \rho m v_{\alpha} v_{\beta} - \sigma_{\alpha\beta}^{t}\right)$$

$$T\dot{S} = \int d\mathbf{r} \left\{-\frac{\partial}{\partial t} \left(\frac{1}{2}\rho m \mathbf{v}^{2}\right) - \mu \frac{\partial \rho}{\partial t} + h_{\alpha} \dot{p}_{\alpha} + r\Delta \mu\right\}.$$

$$\frac{\partial \rho}{\partial t} + \nabla \cdot (\rho \mathbf{v}) = 0.$$

$$\text{where}$$

$$\sigma_{\alpha\beta}^{t} = \sigma_{\alpha\beta} + \sigma_{\alpha\beta}^{A} - \delta_{\alpha\beta} P,$$

$$P_{\alpha} = \frac{Dp_{\alpha}}{Dt} = \frac{\partial p_{\alpha}}{\partial t} + v_{\beta} \partial_{\beta} p_{\alpha} + \omega_{\alpha\beta} p_{\beta}$$

$$v_{\alpha\beta} = \frac{1}{2} (\partial_{\alpha} v_{\beta} + \partial_{\beta} v_{\alpha}),$$

$$\omega_{\alpha\beta} = \frac{1}{3} (\partial_{\alpha} v_{\beta} - \partial_{\beta} v_{\alpha}).$$

(d): same sig. under time reversal

(r): opposite sig. under time reversal

Flux	Force
$\sigma_{lphaeta} = \sigma_{lphaeta}^r + \sigma_{lphaeta}^d, \ P_{lpha} = P_{lpha}^r + P_{lpha}^d, \ r = r^r + r^d$	$v_{lphaeta}$
$P_{\alpha} = P_{\alpha}^{r} + P_{\alpha}^{d},$	$h_{lpha}$
$r = r^r + r^d$ .	$\Delta \mu$

# How to couple thermodynamic forces and fluxes?

- \* Linear Onsager expansion
- \* Respect symmetries of the system

# How to couple thermodynamic forces and fluxes?

1. **Spatial symmetry**: The tensorial character of the Onsager expansion should be conserved.

- 2. Time-reversal symmetry:
- a. Dissipative flux: fluxes and forces with same time signature couples.
- b. Reactive flux: fluxes and forces with opposite time signature couples.

### 'Wet' Active Matters or 'Active Gel'

(description of *slightly* active *polar* gel)

Linear Onsager expansion..

# Dissipative flux (flux and force with same time sig.)

$$P_{\alpha}^{d} = \frac{h_{\alpha}}{\gamma_{1}} + \epsilon p_{\alpha} \Delta \mu,$$

$$r^d = \Lambda \Delta \mu + \epsilon p_\alpha h_\alpha.$$

$$\sigma^d = ar{\eta} u, \ ilde{\sigma}^d_{lphaeta} = 2 \eta ilde{v}_{lphaeta}.$$

# Reactive flux (flux and force with opposite time sig.)

$$\begin{split} \sigma^r &= -\bar{\xi}\Delta\mu + \bar{\nu}_1 p_\alpha h_\alpha, \\ \tilde{\sigma}^r_{\alpha\beta} &= -\zeta\Delta\mu q_{\alpha\beta} \\ &\quad + \frac{\nu_1}{2} \bigg( p_\alpha h_\beta + p_\beta h_\alpha - \frac{2}{3} p_\gamma h_\gamma \delta_{\alpha\beta} \bigg), \\ P^r_\alpha &= -\bar{\nu}_1 p_\alpha \frac{u}{3} - \nu_1 p_\beta \tilde{v}_{\alpha\beta}, \\ r^r &= \bar{\zeta} \frac{u}{3} + \zeta q_{\alpha\beta} \tilde{v}_{\alpha\beta}. \end{split}$$

$$q_{\alpha\beta} = p_{\alpha}p_{\beta} - \frac{1}{3}\delta_{\alpha\beta}$$

### 'Wet' Active Matters or 'Active Gel'

(description of *slightly* active *polar* gel)

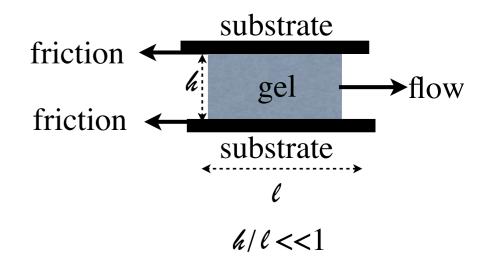
Viscoelastic constitutive eq. (compressible, apolar, isotropic active gel)

$$\left(1 + \tau \frac{D}{Dt}\right) \left(\sigma_{\alpha\beta} - \zeta \Delta \mu \delta_{\alpha\beta}\right) = \eta(\partial_{\alpha} v_{\beta} + \partial_{\beta} v_{\alpha}) + \eta_{b} \partial_{\gamma} v_{\gamma} \delta_{\alpha\beta}$$

### **Active Gel with Substrate**

(momentum balance)

$$\nabla . \sigma = \gamma \mathbf{v}$$



$$dry \leftarrow (small) \quad \eta/\gamma \quad (large) \quad Wet$$

G. Salbreux et. al.

Phys. Rev. Lett.(2009).

### **Dynamics of Myosin Density**

rate of change of density profile = advection of the density profile with flow + source term

$$\frac{\partial c}{\partial t} = D\nabla^2 c - \nabla \cdot (\vec{v}c) + \frac{c_0 - c}{\tau_a}$$

# **Physical Principles**

- 1. stress ~ viscous strain rate
- 2. stress ~ elastic strain
- 3. total strain = viscous strain + elastic strain
- 4. total stress = passive stress + active stress

1. rate of change of height profile = advection of the density profile with flow + wound healing

**Dynamics of density** 

**Constitutive Eq.** 

1. cortex - a 'thin film'

2. gradient of stress ~ flow velocity

Force balance

### **Theoretical Model**

#### Material properties:

Shear viscosity  $\eta$ 

Bulk viscosity  $\eta_b$ 

Time constant for viscoelastic relaxation  $\tau$ 

Time constant for turning over of cortex  $\tau_a$ 

Friction coefficient  $\gamma$ 

Active contractility  $\xi$ 

#### Dynamical variables

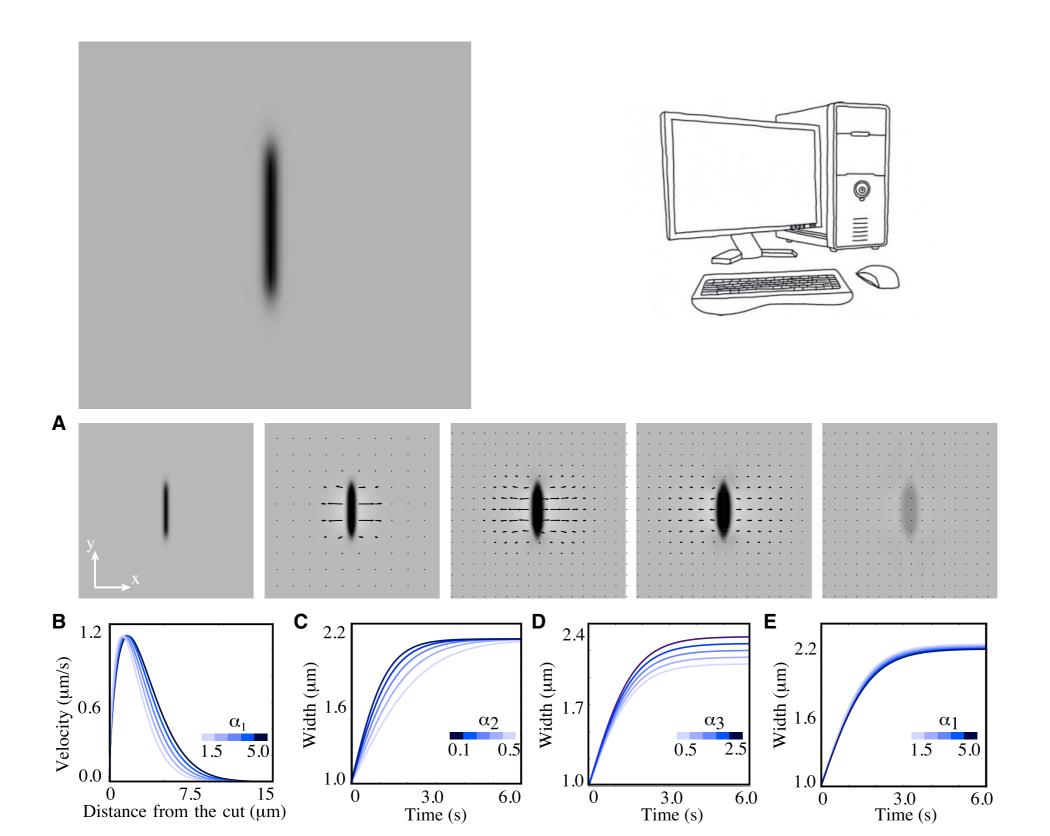
Density

Velocity  $v_{\alpha}$ 

Stress (active and passive)  $\sigma_{\alpha\beta}$ ,  $\sigma^a \delta_{\alpha\beta}$ 

### Perturbation to the Fluid to Estimate the Material Properties

### **Laser ablation : Theory**



### To Estimate Material Properties....

Find Independent Parameters of the theory.



Solve the model equations with laser ablation as initial condition to have the cut responses as in experiment.



Minimize the difference between all the experimental and theoretical cut responses simultaneously with the independent parameters. Note the values of the parameters where the difference is minimum.



From these values, find the material parameters.

### Dimensionless Free Parameters of the Model

$$\alpha_1 = \frac{\lambda_c}{\lambda}$$

$$\lambda_c = \text{cut length}$$

$$\alpha_2 = \frac{\tau}{\tau_a}$$

$$(\lambda = \text{hydrodynamic length} = \sqrt{\frac{\eta}{\gamma}})$$

$$\alpha_3 = \frac{\xi^a \tau_a}{\gamma \lambda_c^2}$$

### **Global Fitting of Response Curves**

Squared distance between theory (t) and experimental (e) responses of ablation:

$$\Delta(\alpha_i) = \sum_{l} \left( \frac{I_e^l - I_t}{\sigma_I^l} \right)^2 + \sum_{m} \left( \frac{V_e^m - V_t}{\sigma_V^m} \right)^2 + \sum_{n} \left( \frac{W_e^n - W_t}{\sigma_W^n} \right)^2$$

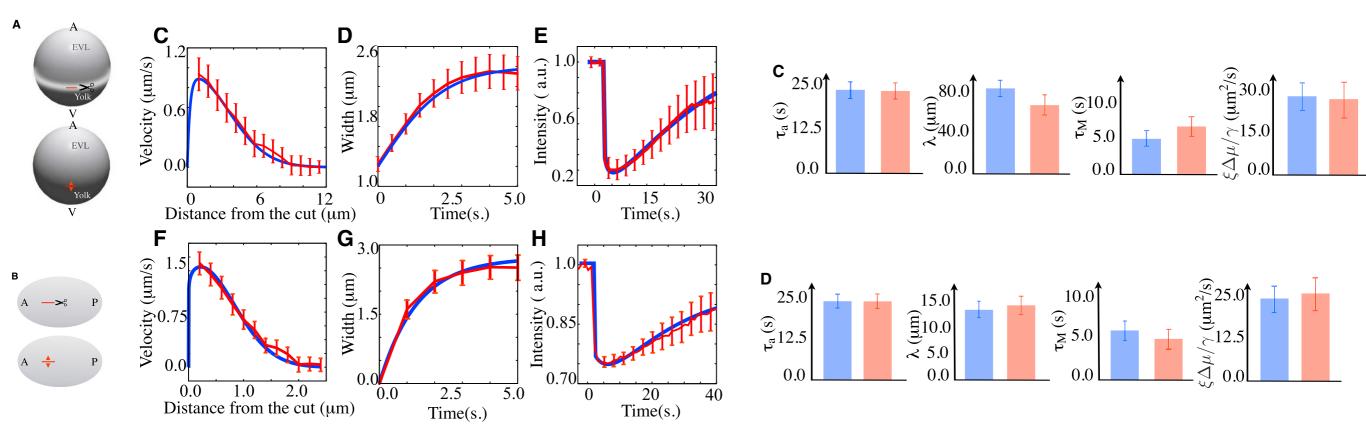
Intensity / density difference

Velocity profile difference

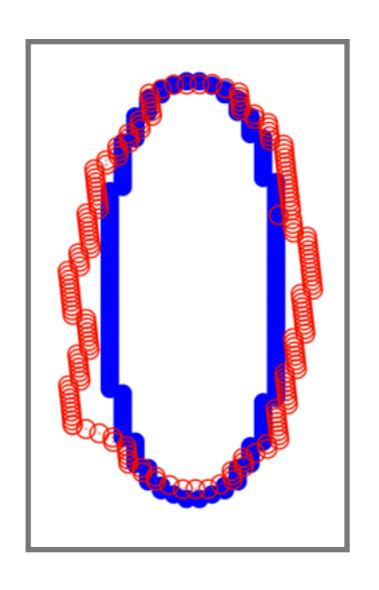
Width of the cut difference

$$\{\alpha_i\} \to (\alpha_1, \alpha_2, \alpha_3, \tau_a)$$

### **Material Parameters**



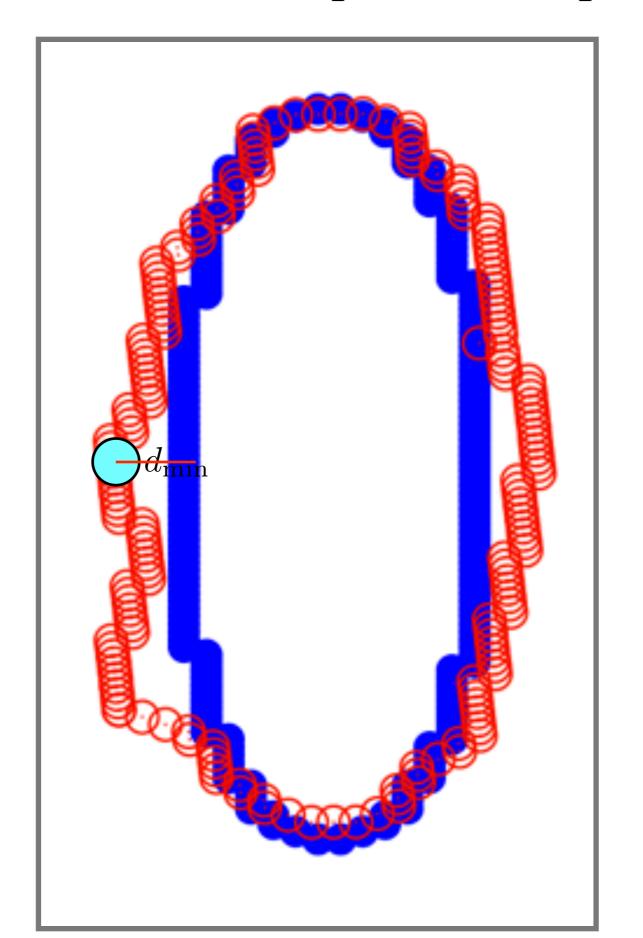
### **Evolution of the Shape of the Hole**



Shape: Experiment

Shape: Theory

### 'Distance' Between Shapes from Experiment and Theory



Boundary points: Experiment

Boundary points: Theory

$$S = \sum d_{min}^e$$

### Minimization of the 'Distance'

$$\bullet \ \frac{\partial S}{\partial \alpha_i} = 0$$

$$\bullet S(\{\alpha_i\} = \{\alpha_i^*\}) = S_{\min}$$

$$At \{\alpha_i\} = \{\alpha_i^*\}$$

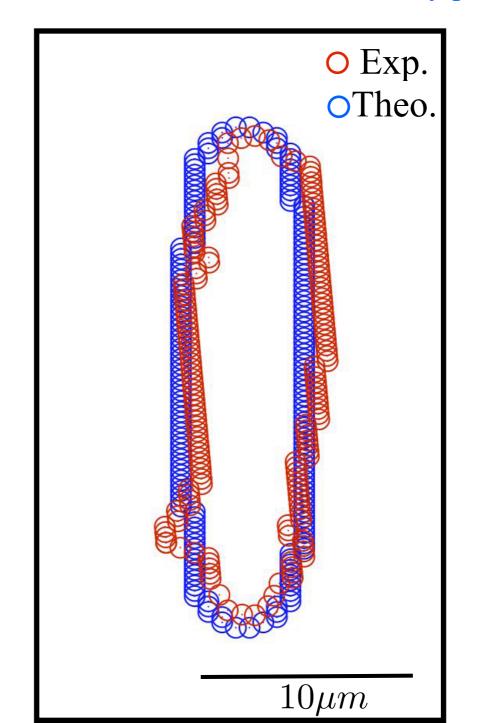
$$\alpha_1 = \frac{\lambda_c}{\lambda} = \alpha_1^*$$

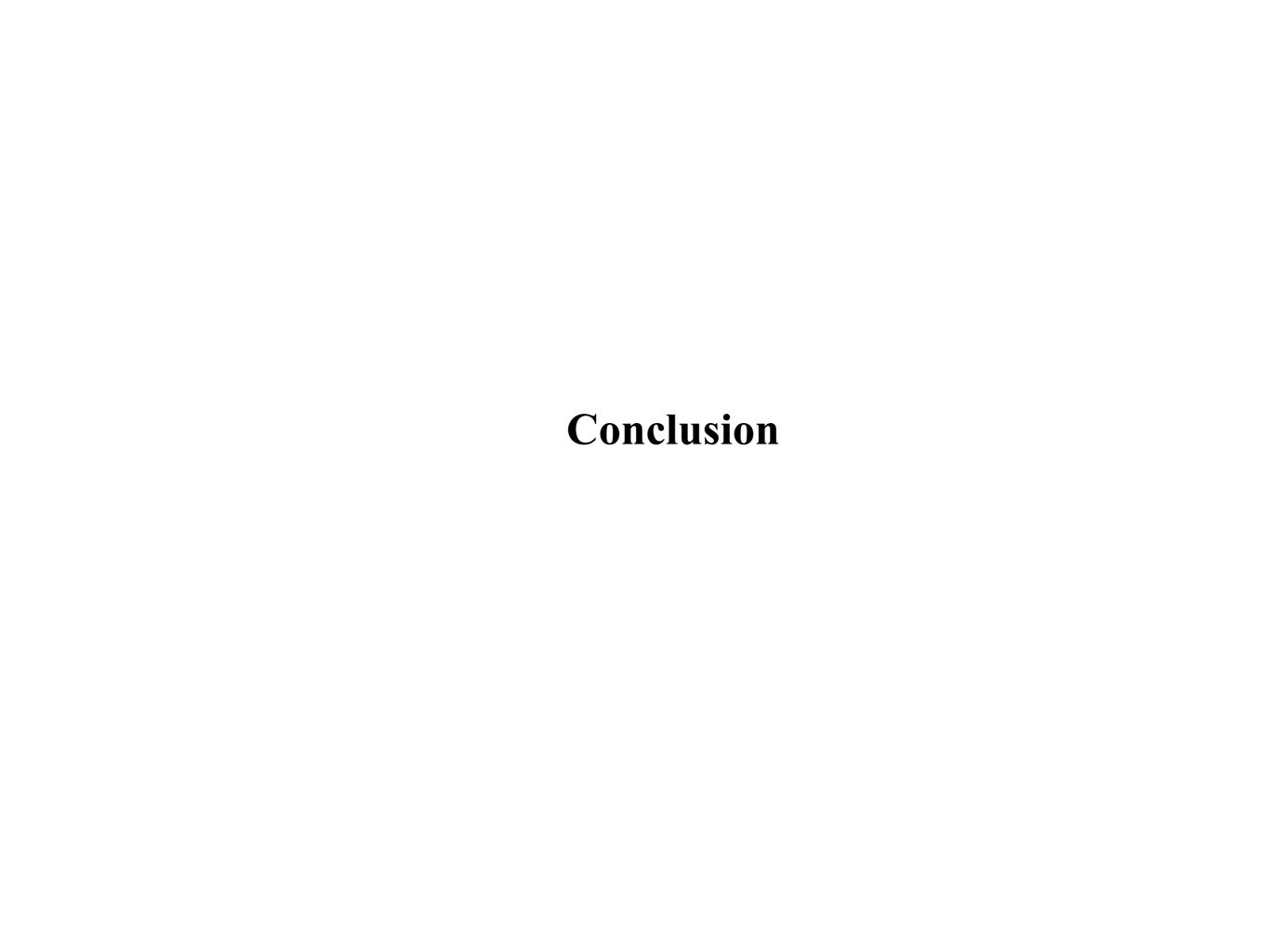
$$\alpha_2 = \frac{\tau}{\tau_a} = \alpha_2^*$$

$$\alpha_3 = \frac{\xi^a \tau_a}{\gamma \lambda_c^2} = \alpha_3^*$$

Boundary points: Experiment

Boundary points: Theory





## Acknowledgements



**Division Biological Physics** 



Grill-lab



Heisenberg-group